

Technology Transition Workshop | *Mohamed R. Mahfouz, Ph.D.*

History and Application of Computed Tomography (CT) Images

Outline

- **Why 3D?**
- **CT Principles**
- **Calibration**
- **Modeling**
- **Applications**

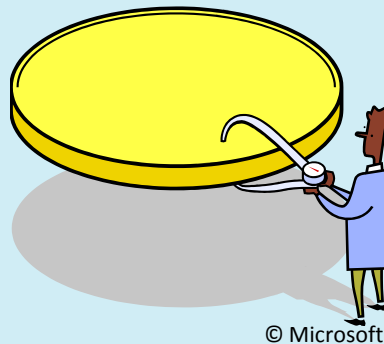
Why 3D?

Conventional Methods

- X-Ray

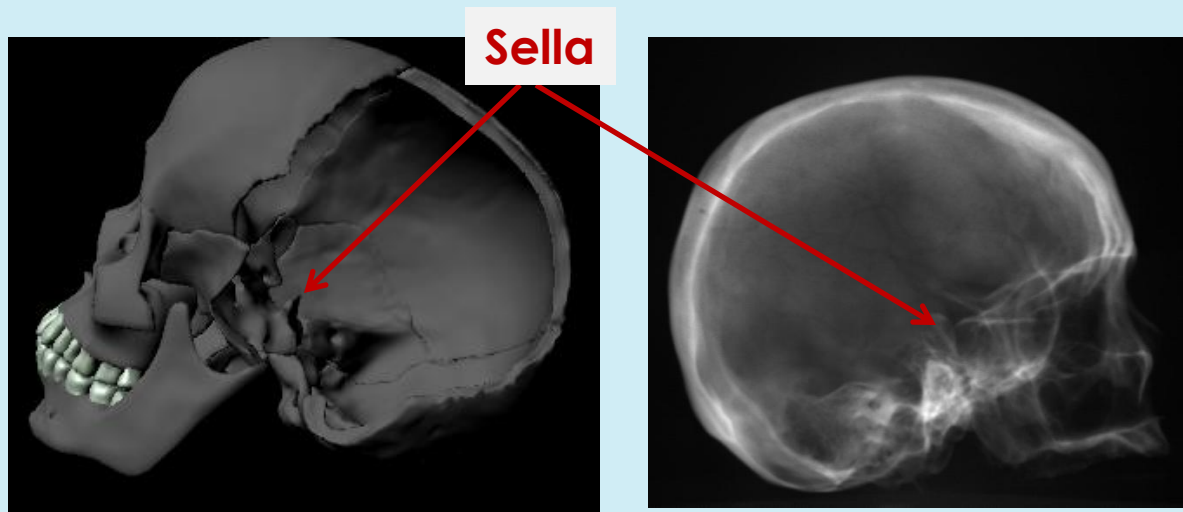


- Calipers



X-Ray

- **2D Projection of 3D Anatomy**
 - Dense object can shadow structure behind it
 - No depth perception
 - Projection change by rotating object relative to imaging plane
 - Limited soft tissue information

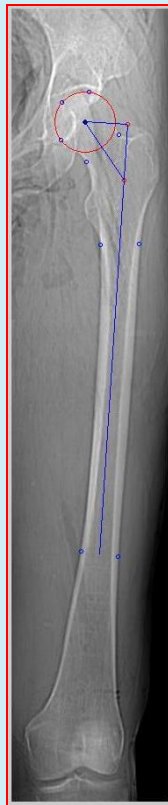


X-Ray Accuracy

Female Case

X-Ray Proximal Angle = 142.78

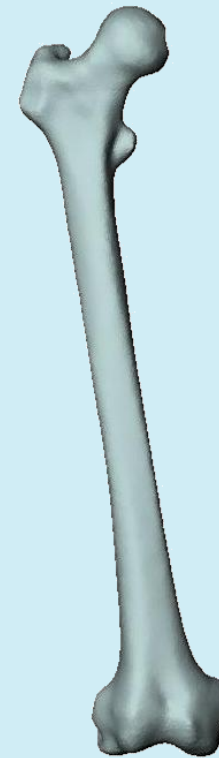
True 3D proximal angle = 130.84



Male Case

X-Ray Proximal Angle = 140.16

True 3D proximal angle = 127.62



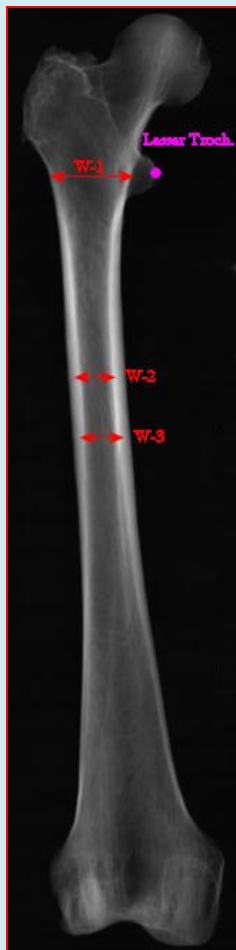
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Effect Of Rotation on X-Ray



Effect Of Rotation on X-Ray



2-D Measurements

	W-1	W-2	W-3
μ	7.90%	4.62%	2.25%
σ	5.90%	3.01%	2.51%

Percentage Error in 2-D Measurements
Due to 12° External Rotation

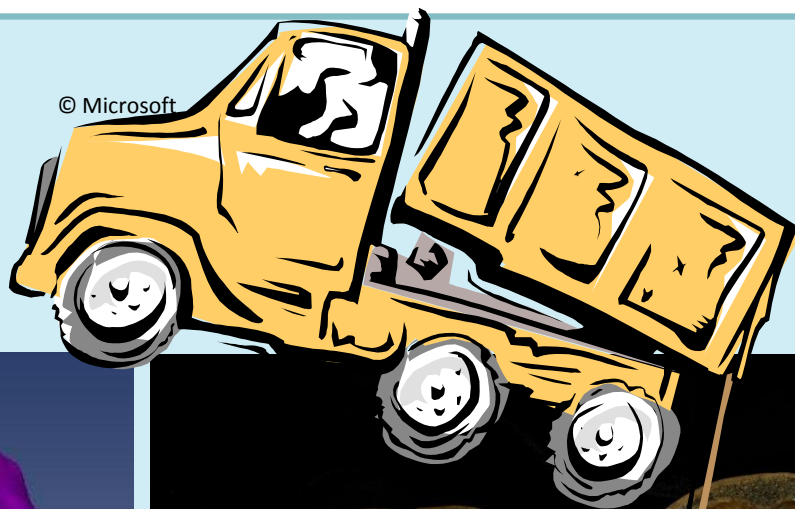
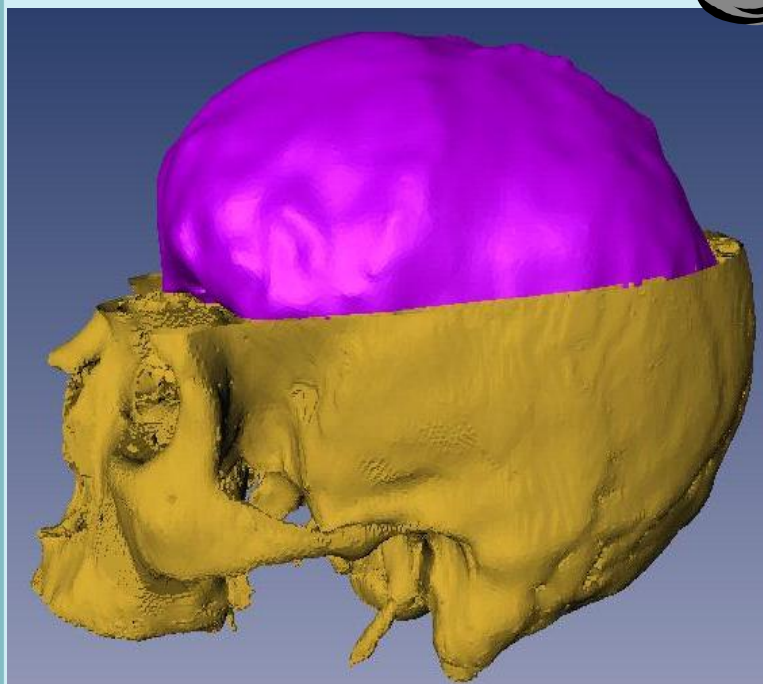
	W-1	W-2	W-3
μ	5.84%	3.83%	1.41%
σ	6.23%	1.73%	1.75%

Percentage Error in 2-D Measurements
Due to 10° Internal Rotation

Calipers

- **Intra- and inter-observer error**
- **Can be only used for geodesic measurements**
- **Limited access to anatomical features**
 - **Finding internal landmarks (autopsy)**
 - **Limited number of landmarks**
- **Time consuming**

Calipers



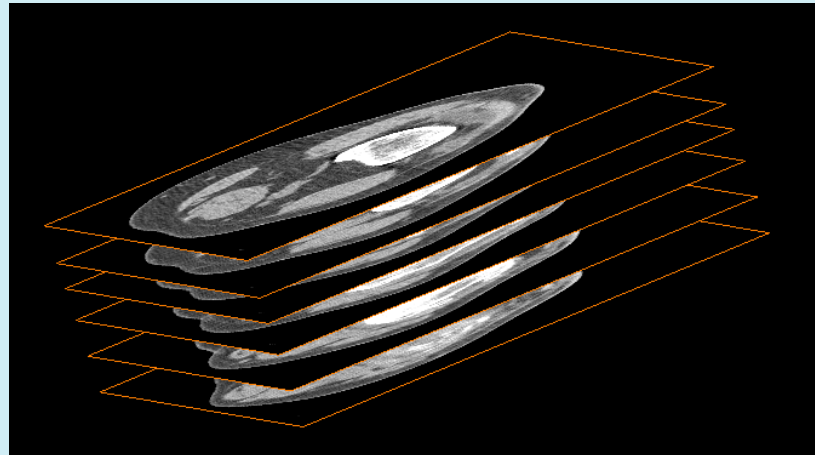
How To Measure Volume???

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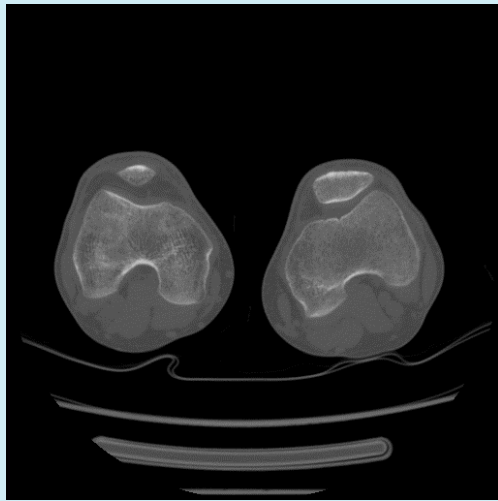
CT

- **What's a CT?**
 - **X-Ray device capable of imaging cross sections of object**
 - **Create stack of images; each represents slice from object**
 - **Images stacks can be arranged in 3D to create volume**



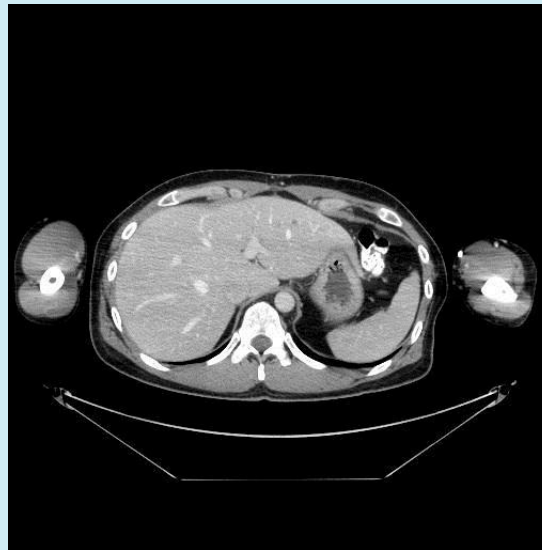
CT Applications

- **Wide range of applications in both soft tissue and bones**



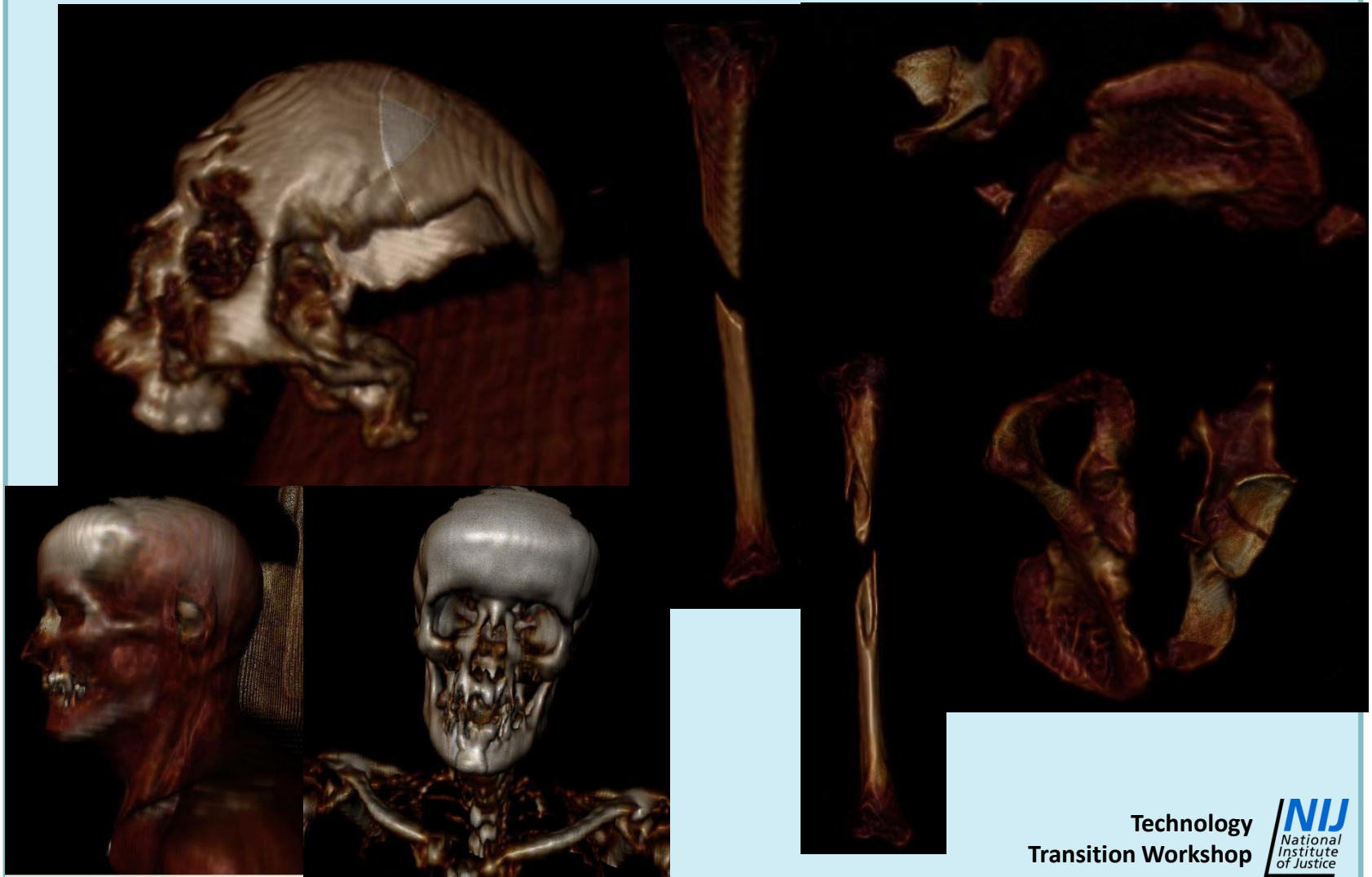
Knee

Lumbar



Hip

CT Applications



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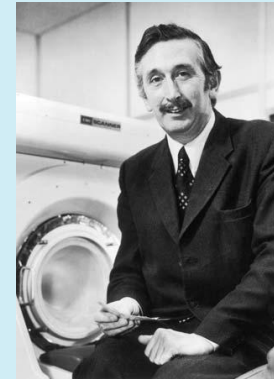


CT History

- **Computed tomography (CT) became the historically first tomographic modality entirely based on digital reconstruction of images**
- **Medical image reconstruction refers to the reconstruction of cross sectional or volume data from the projection data at various angles**
- **Introduced by Hounsfield and Cormack**
- **Nobel Price 1979 (Physiology or Medicine)**

Sir Godfrey Newbold Hounsfield
1919-2004

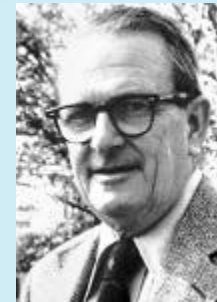
Nobel Price for Medicine : 1979



© Vanderbilt University Medical Center

Prof. Allan McLeod Cormack
1924-1998

Nobel Price for Medicine : 1979

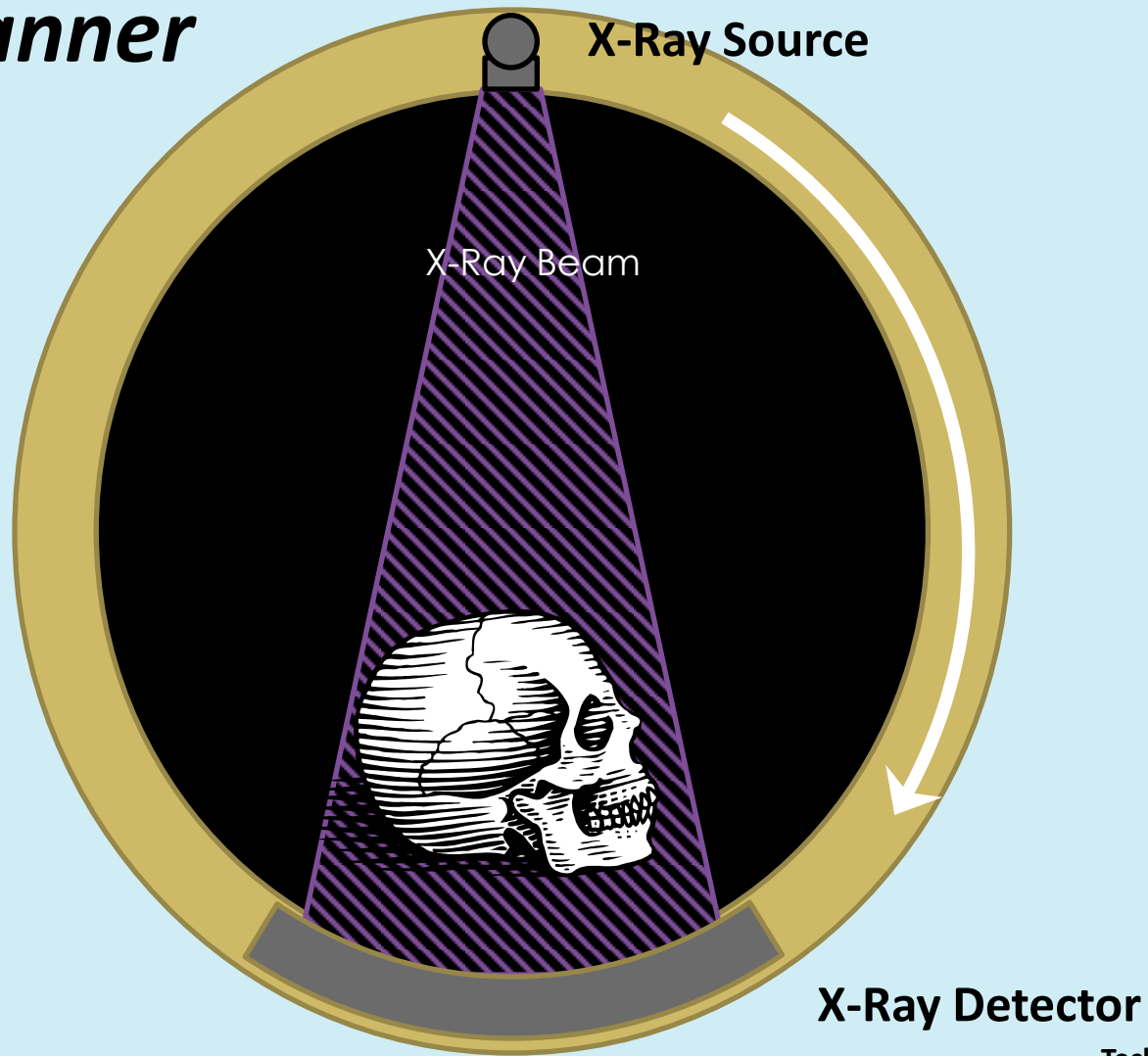


Courtesy of Freebase.com

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CT Scanner



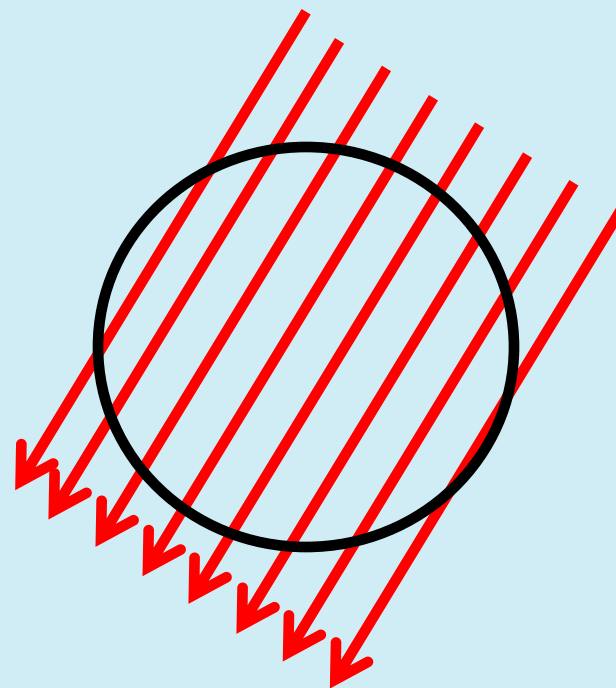
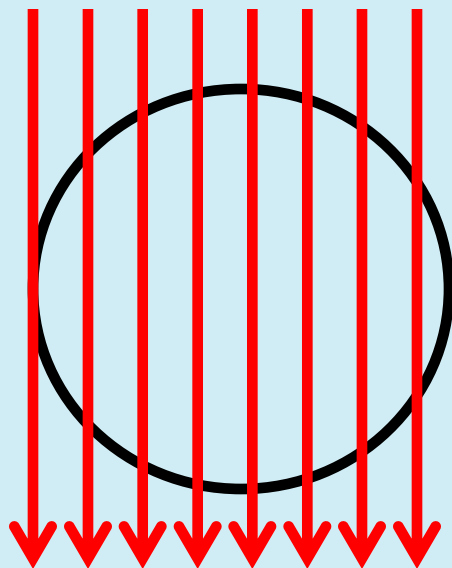
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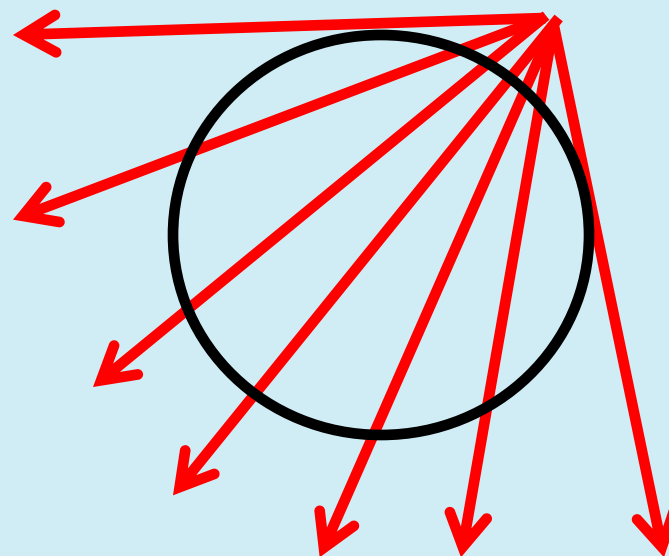
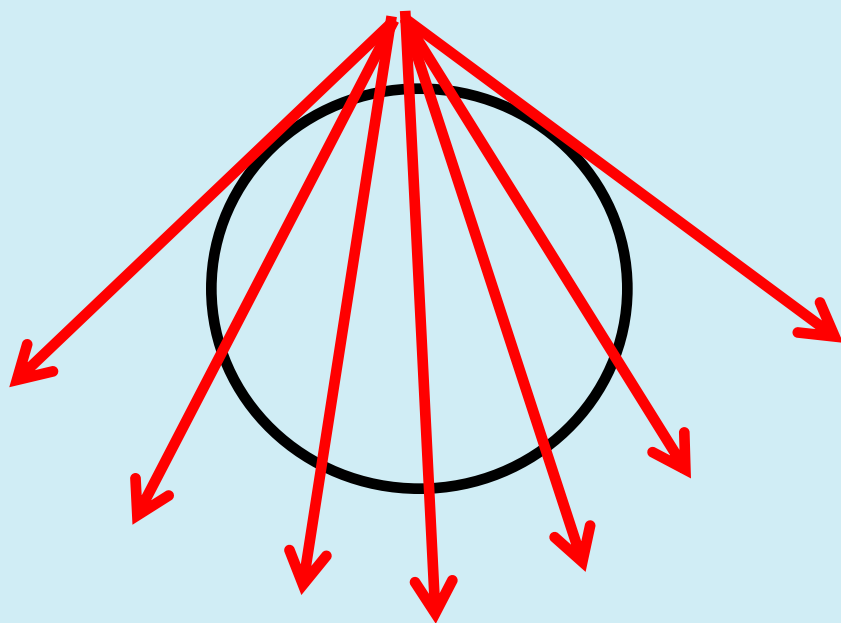
Basic Idea

- **2D views (projections) at all angles around the patient**
 - **Rotating source and detector**
 - **Sample attenuation at each detector for each angle**
 - **Generate projections**
 - **Different beam geometry**
 - **Parallel**
 - **Fan**
 - **Cone**

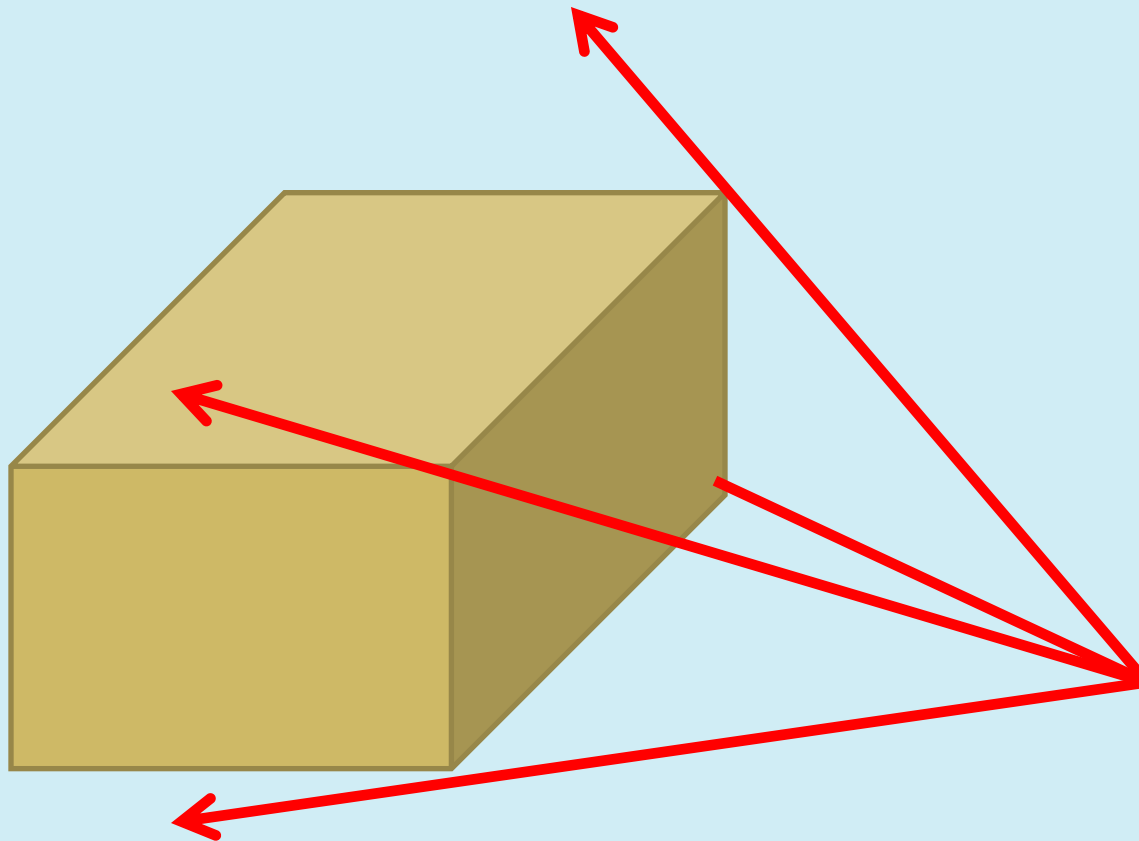
Parallel Beam



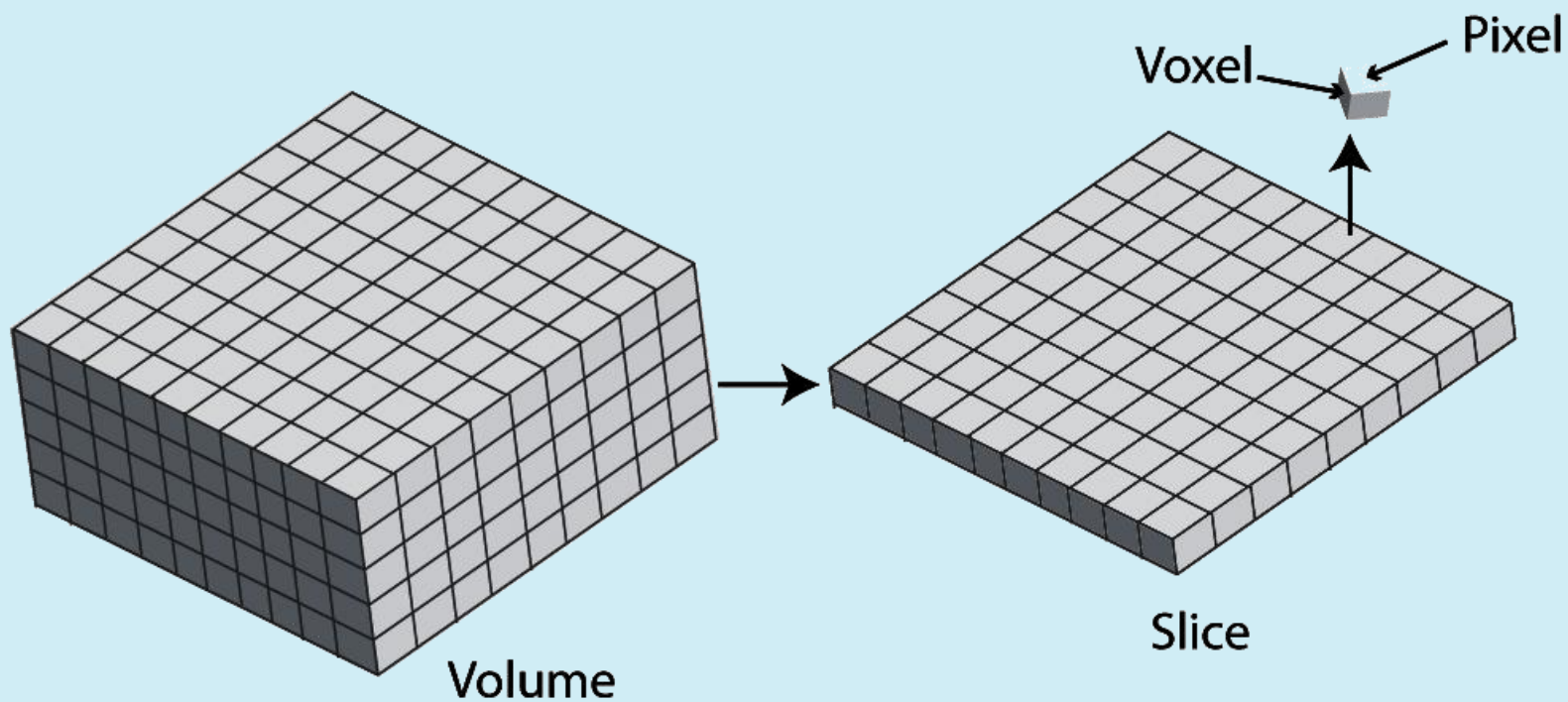
Fan Beam



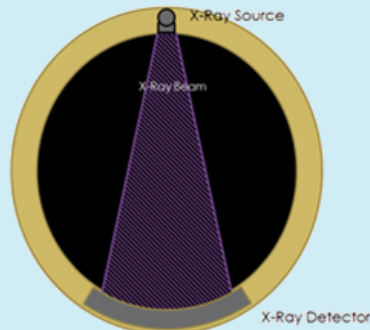
Cone Beam



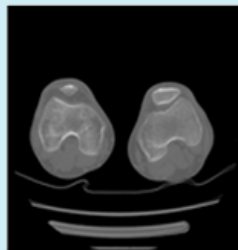
Pixel vs Voxel



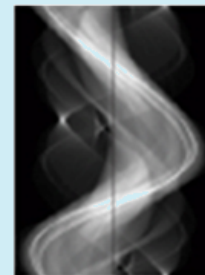
CT Reconstruction



Attenuation Data from rotating source and detector around object



Reconstructed Image



Sinogram: a line for every angle

CT Number

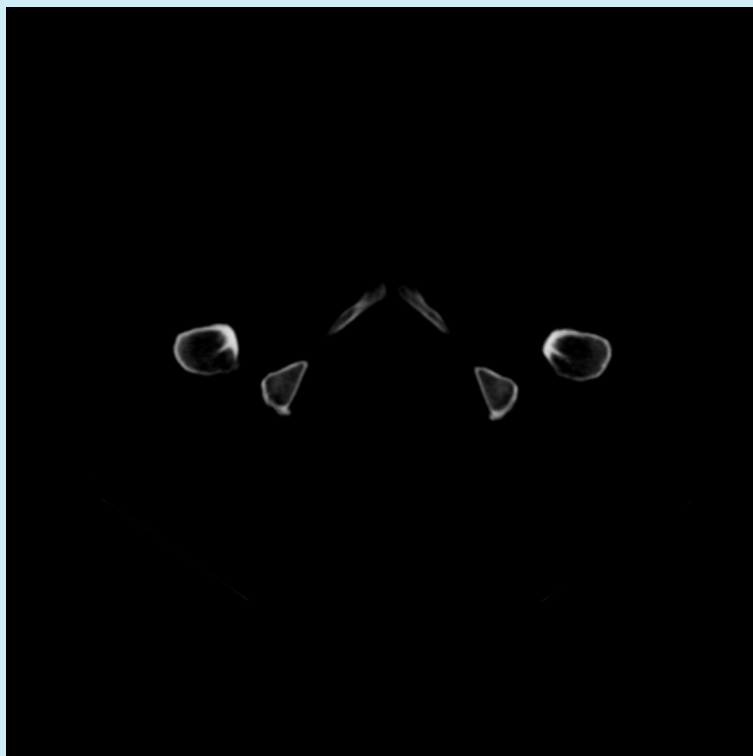
- **Images:**
 - **Size generally 512*512**
 - **Linear attenuation coefficient measured between tube and detector**
 - **Attenuation coefficient measure: how x-ray absorbed with material**
 - **Values in Hounsfield Units (HU)**

$$\text{CT number (HU)} = \frac{\mu - \mu_{H_2O}}{\mu_{H_2O}} * 1000$$

CT Number Window

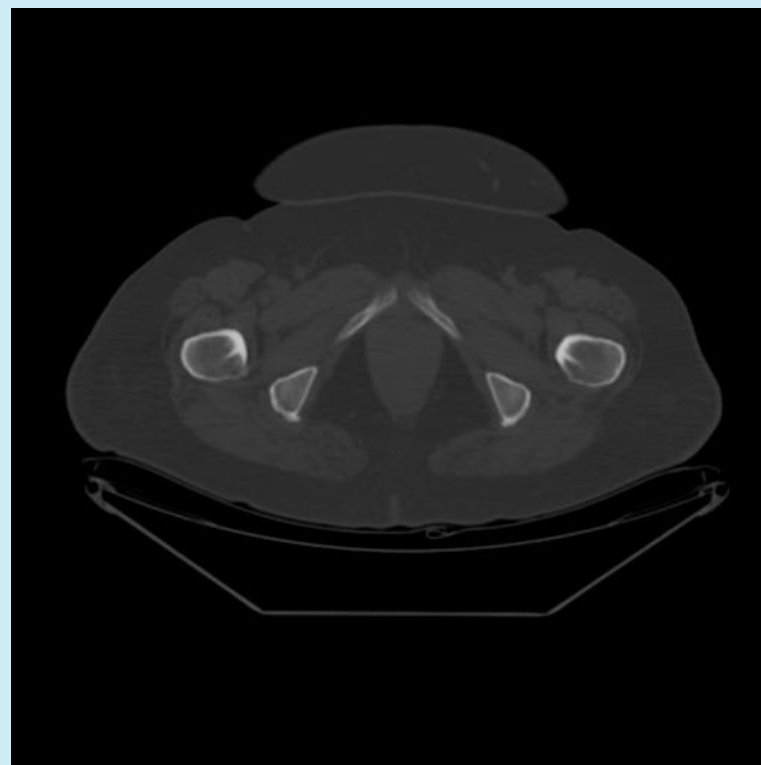
- **Due to large dynamic range, windowing is used to view images**
- **The windowing affects both brightness and contrast**
- **Window is defined by Window Level (WL) and Window Width (WW)**
 - **WL is CT number of the mid gray**
 - **WW is number of HU from black to white**

CT Number Window



WL: 752

WW: 2639



WL: 899

WW: 1531

CT Parameters

- **Acquisition parameters**
 - Determine production of scan data set
- **Reconstruction parameters**
 - Determine presentation of the data

Acquisition Parameters

- **Tube potential**
 - Voltage between cathode and anode
 - Measured in KeV
 - Higher potential accelerates electrons and thus increase x-ray energy
- **Tube current**
 - Current flowing through cathode
 - Measured in mA
 - Larger current increases number of electrons and thus increases beam intensity

Acquisition Parameters (Continued)

- **Scan time**
 - Time taken for tube and detectors to perform complete rotation
 - Longer scan time increases total x-ray count
- **Collimation\slice thickness**
 - Width of CT slice along z-axis
- **Beam filtration**
 - Different beam shaping filter, optimized for different examinations

Reconstruction Parameters

- **Field of view**
 - Size of image in X and Y directions
- **Reconstruction matrix**
 - Usually 512*512
- **Reconstruction filter**
 - Different filters available from smooth (soft tissue) to sharp (bone)

CT Generations

- **1st generation**
 - **Single detector**
 - **Translate – rotate acquisition**
 - **Translate across patient**
 - **Rotates around patient**
 - **Very Slow**
 - **Minutes per slice**

CT Generations (Continued)

- **2nd Generation**
 - **Narrow fan beam (10 degree)**
 - **Multiple detectors**
 - **Rotation and translation**
 - **Slow**
 - **20 seconds per slice**

CT Generations (Continued)

- **3rd Generation**
 - **Wide fan beam**
 - **Multiple detectors (500-1000)**
 - **Rotation only**
 - **Multiple angle acquisition at each position**
 - **Faster**
 - **0.5 second per rotation**

CT Generations (Continued)

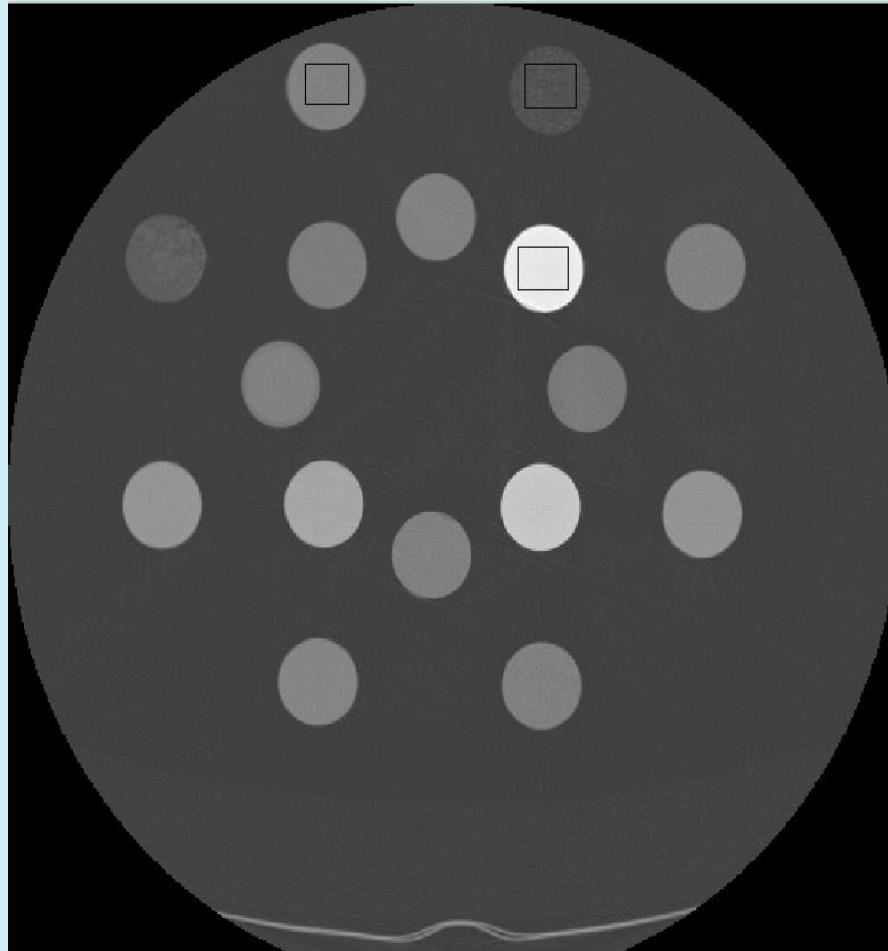
- **4th Generation**
 - Fan beam
 - Static detectors all around gantry
 - Only tube rotates

Calibration Phantom

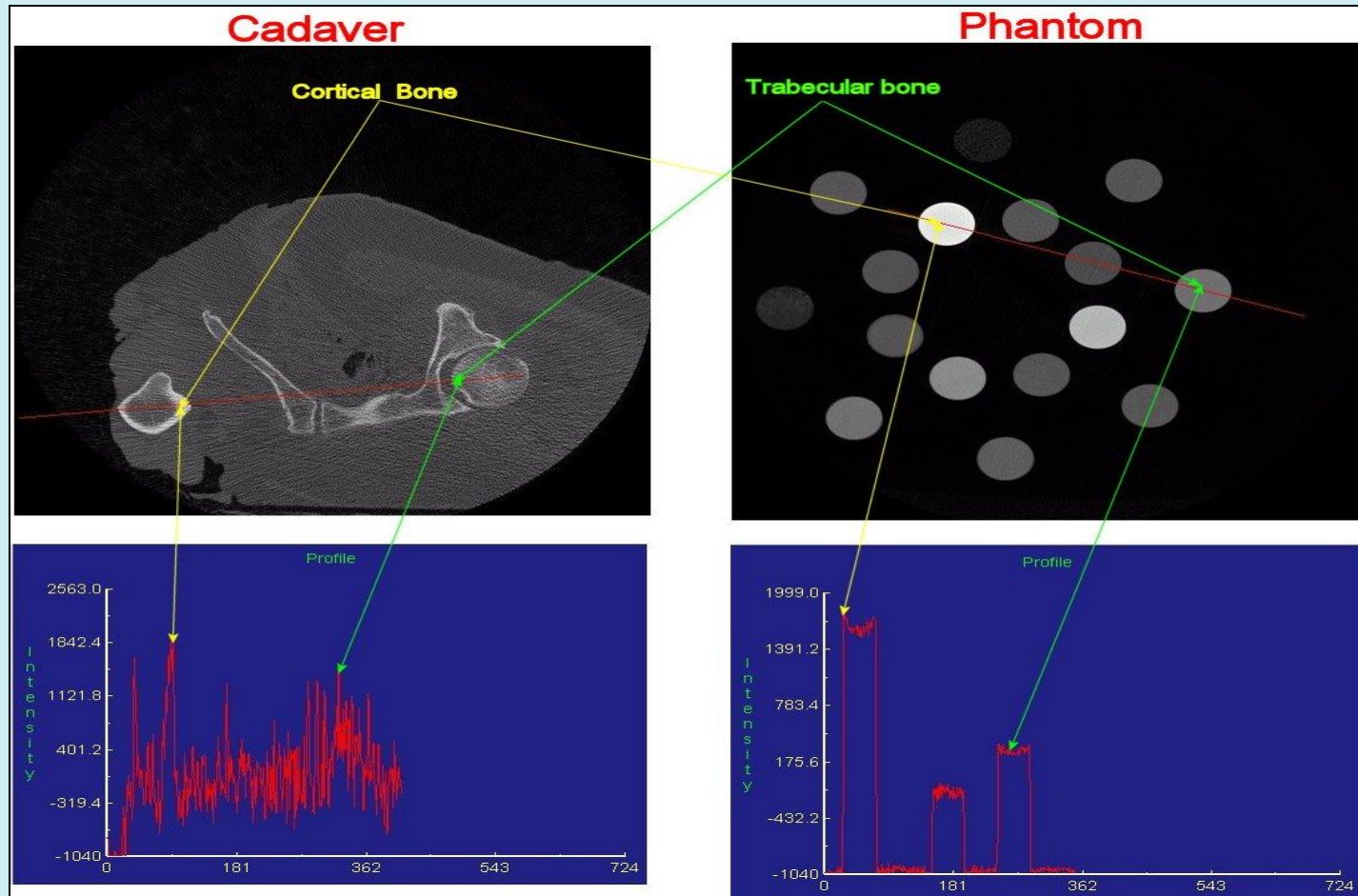
- Has similar properties to human tissue
- Used in procedures for measurement of absorption of radiation
- Used for calculating bone density



CT Image of Phantom



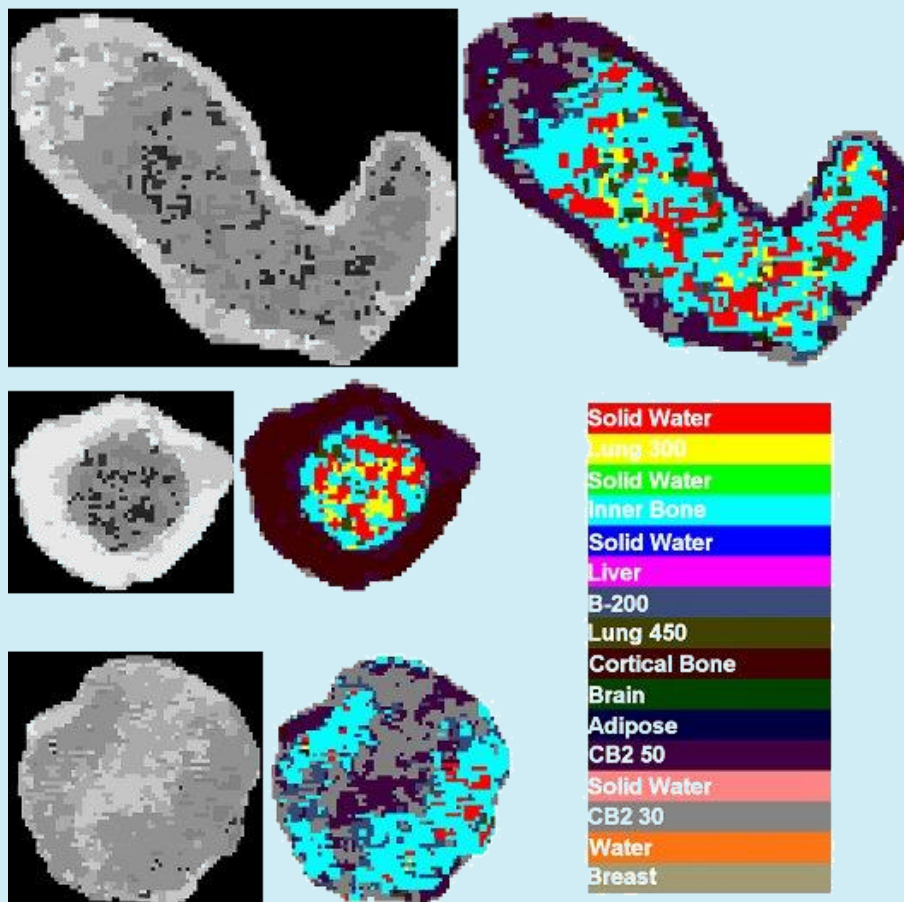
Density Mapping



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Density Mapping



Density and Color Map for Different Parts in Proximal Femur

From Moore, Mahfouz, Abdel Fatah and Badawi (2006).

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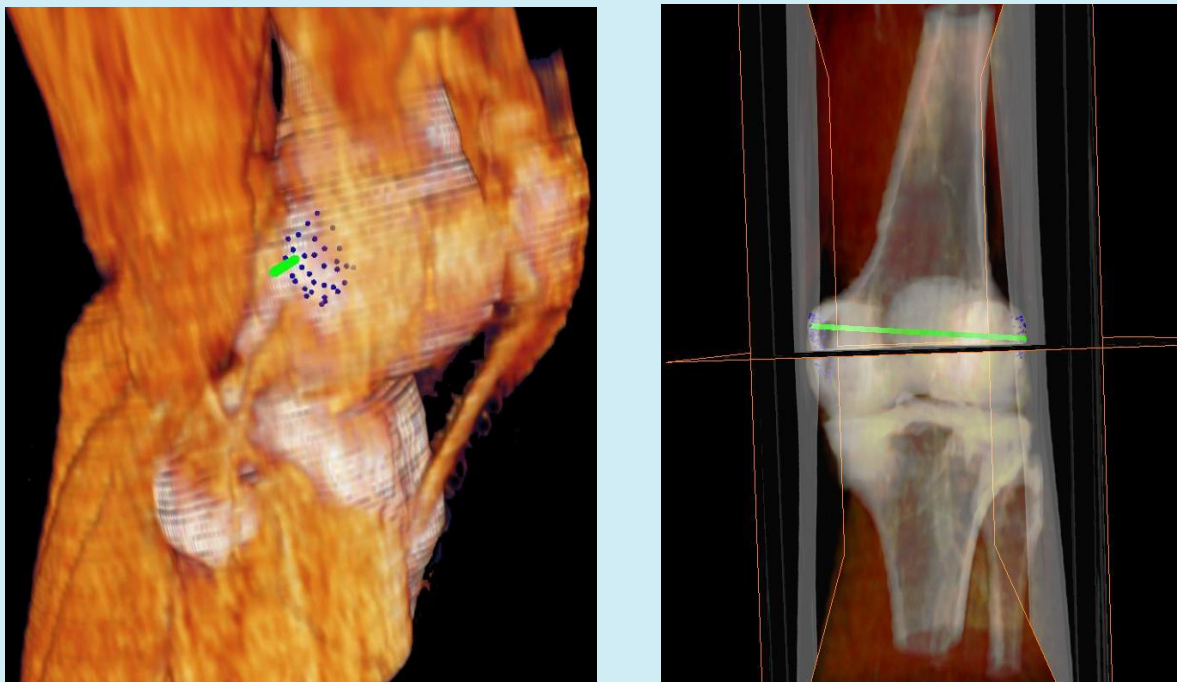
Modeling

Two Methods:

- 1. Directly find landmarks or perform measurements on CT slices**
- 2. Generation of 3D surface model by segmenting object of interest, then perform measurements on the segmented model**

Modeling Directly from CT Slices

- Features can fall between slices

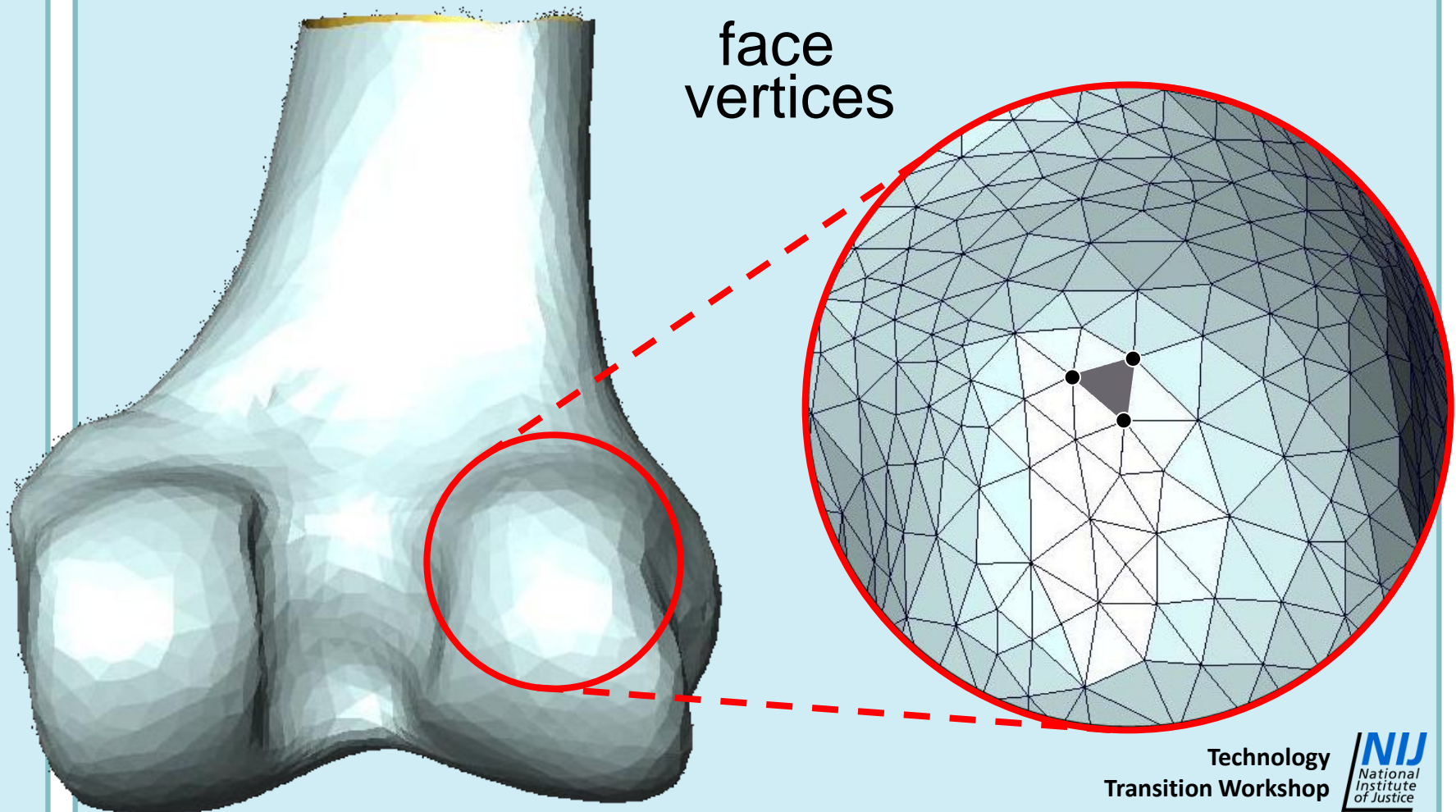


Example: Epicondylar Axis in Femur

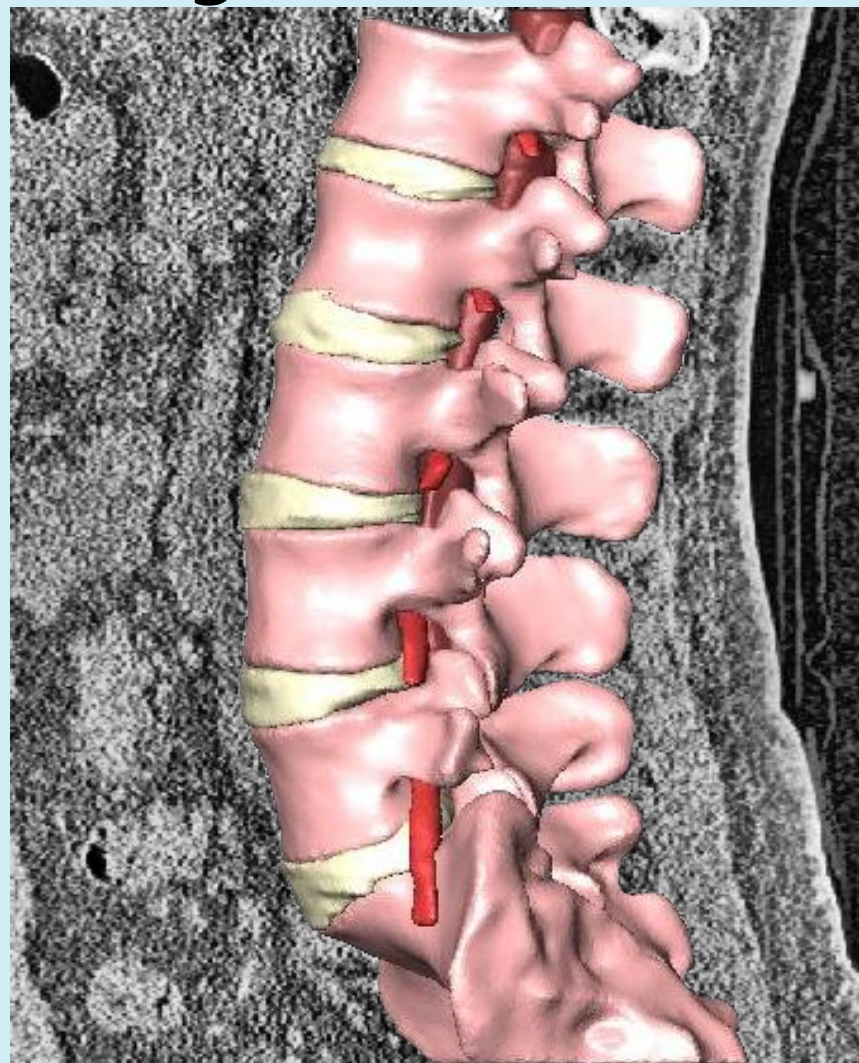
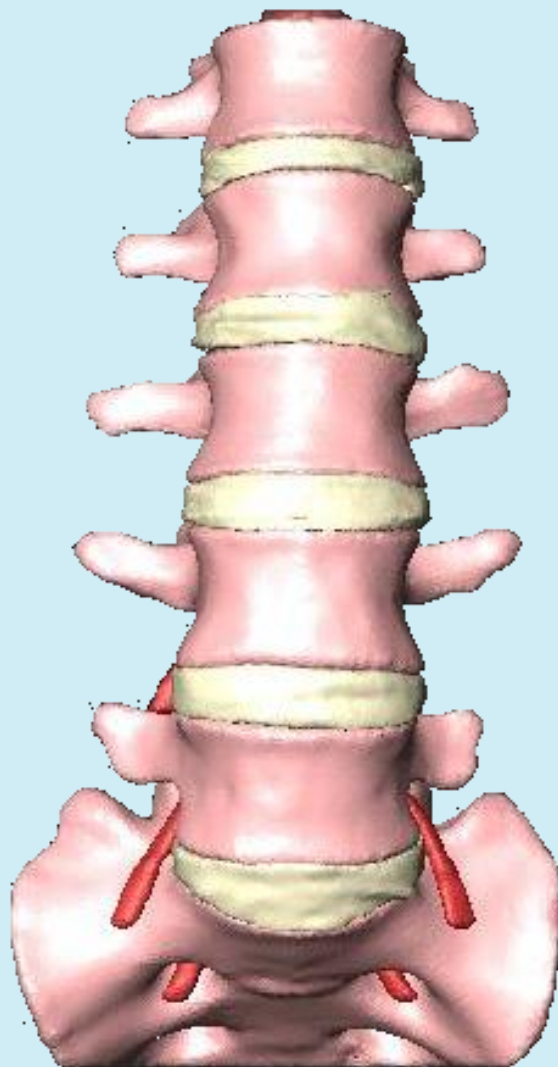
Modeling Using 3D Models

- **Segmentation**
- **Statistical atlases**
- **Reconstructing missing data**
- **Measurements and landmarking**
- **Statistical analysis**

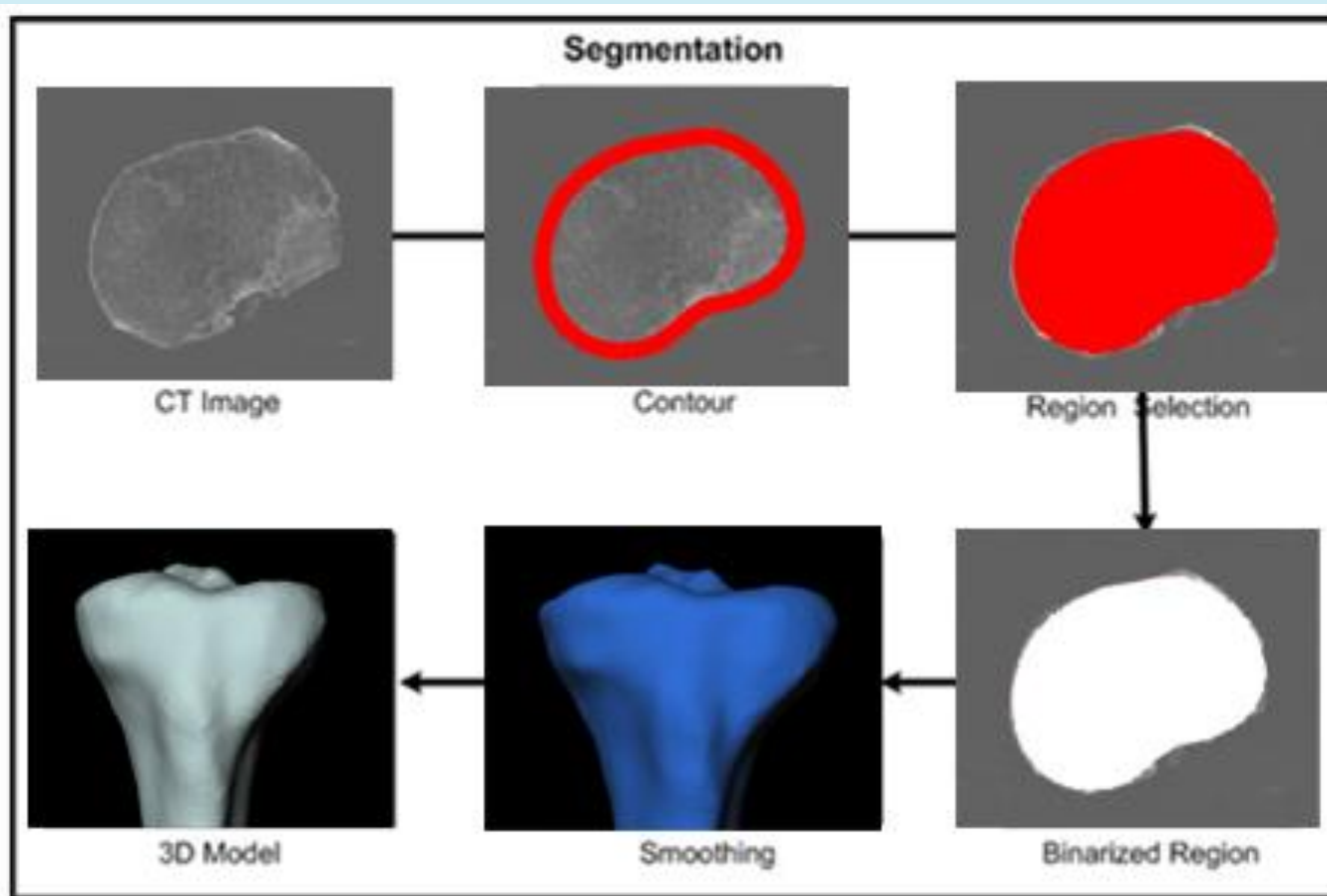
What is a 3D Model?



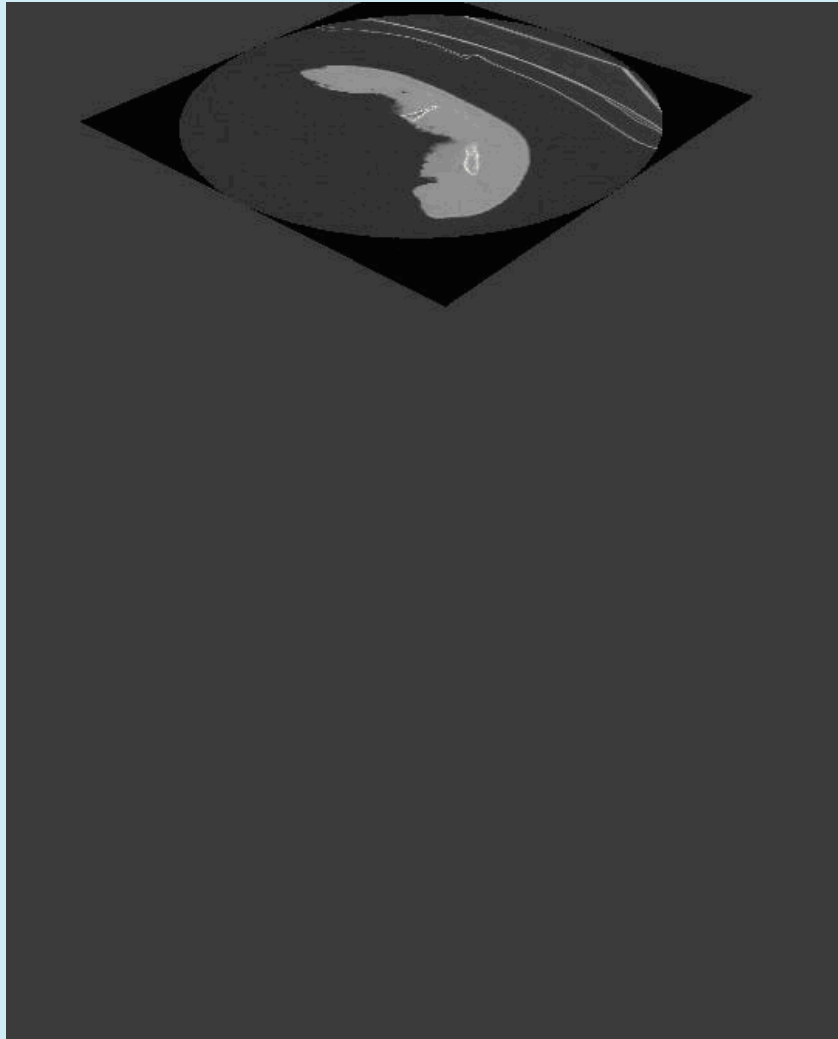
3D Models vs 2D Images



Model Segmentation



Model Segmentation

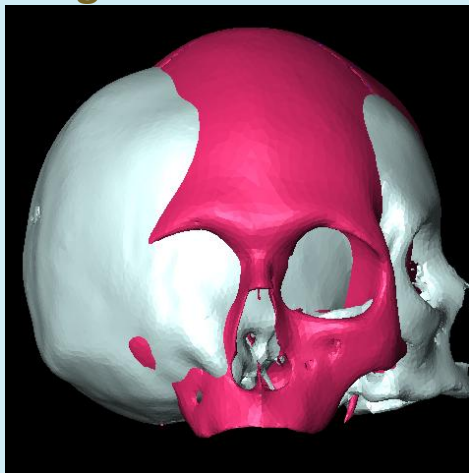


Statistical Bone Atlas

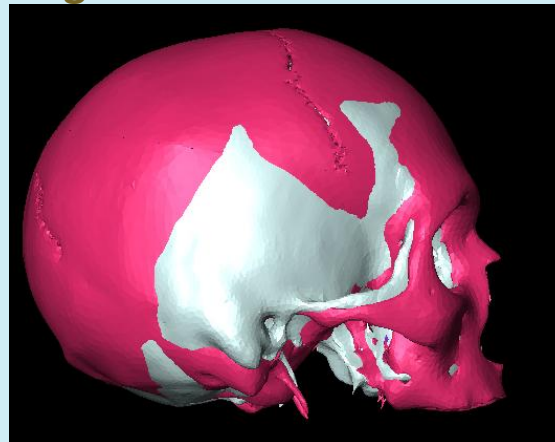
- **Generate surface mesh models built from computed tomography data**
 - New models are converted to a normalized mesh
 - Models then represented with principal components that govern bone shape
- **Statistical variation of morphology can be computed for a population of bones**
- **“Average” bone model computed from bones in the atlas**

Statistical Atlas

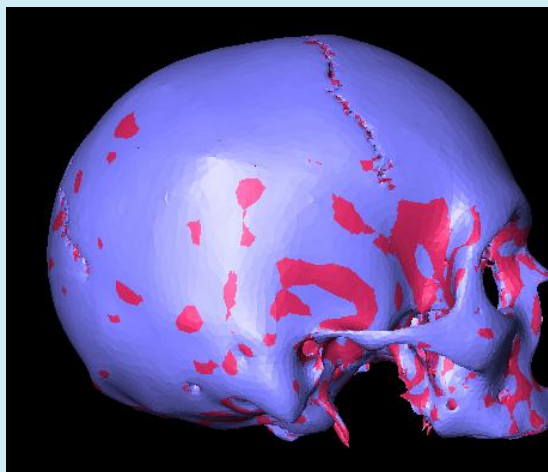
Align bone centroids



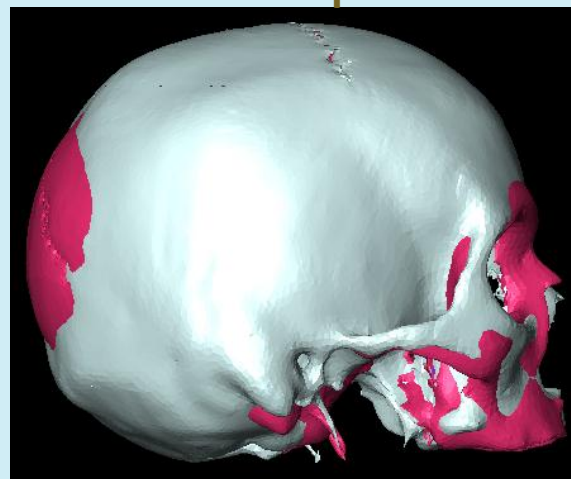
Perform Rigid Iterative Closest Point (ICP)



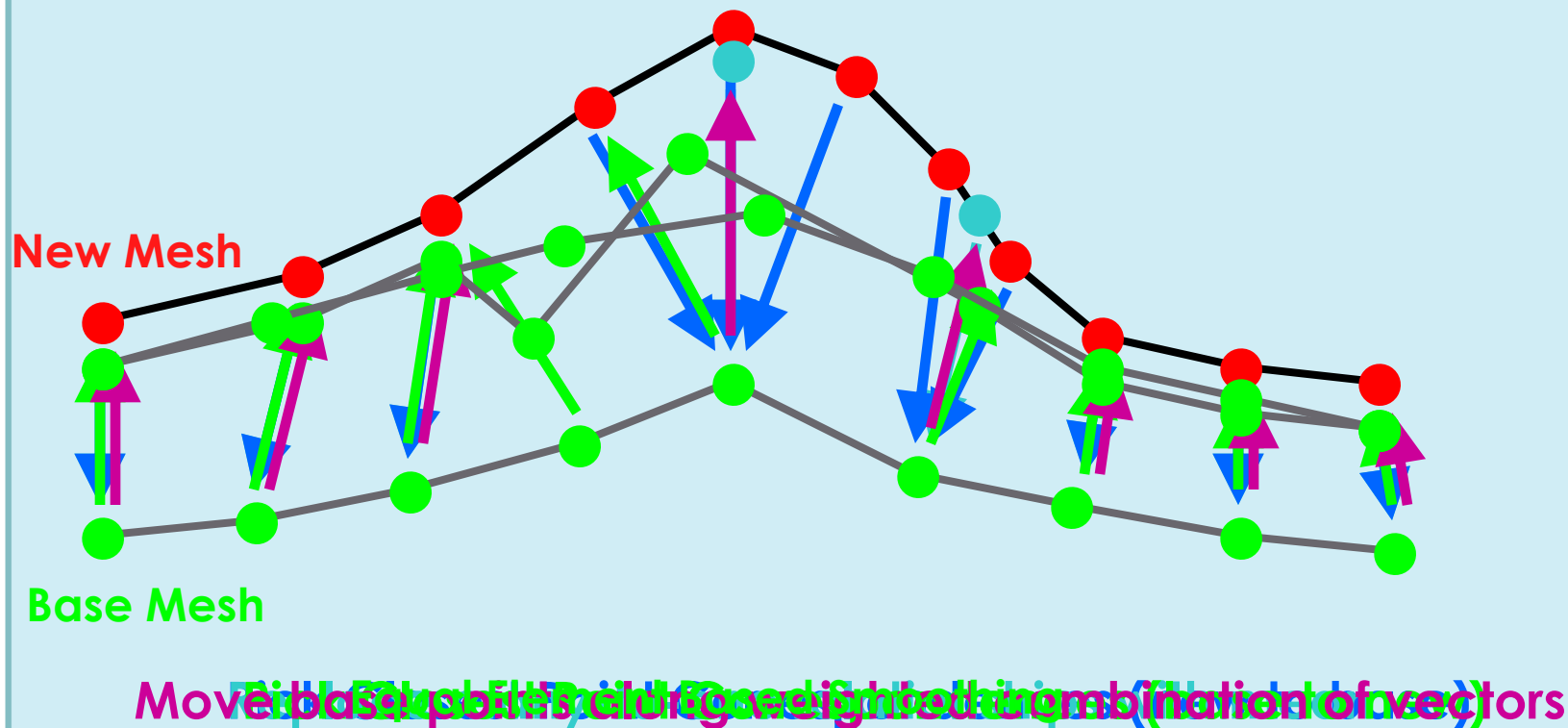
Free Form Transformation



Surface Correspondence



Surface Correspondence



Feature Extraction Techniques

***Statistical
Shape Model***

**Principal
Components
(PCA)**

(Global)

***Specific
Landmarks***

Measurements

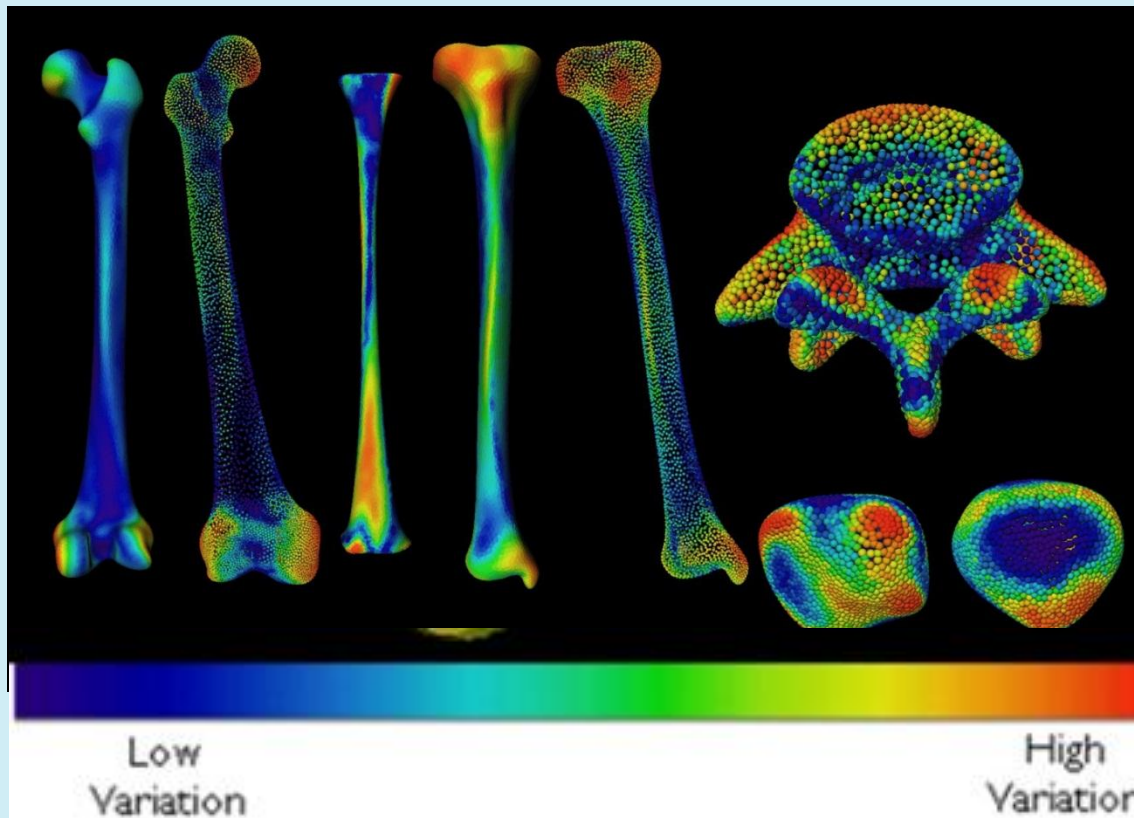
(Local)

Statistical Representation

- **Landmark-Based**
 - **Disadvantage: manually defined landmarks**
 - **Disadvantage: time-consuming**
 - **Disadvantage: high intraobserver error**
 - ***Only capture local statistics***
- **Surface-Based**
 - **Advantage: performed on entire bone surface after establishing correspondence**
 - **Advantage: quick and convenient method**
 - **Advantage: eliminates subjectivity and only done once**
 - ***Capture both global and local statistics***

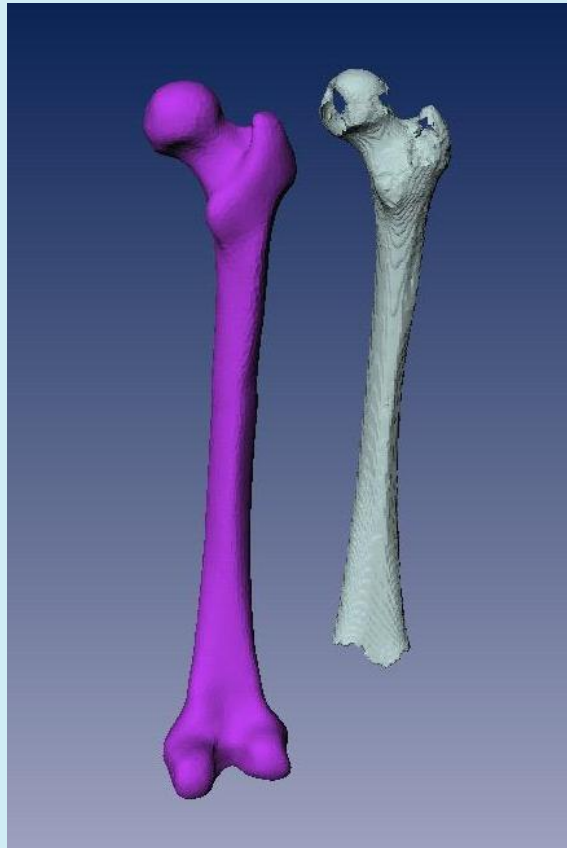
Morphological Differences

- Analysis of differences between gender, ethnicities and ages



Extrapolating Missing Anatomy

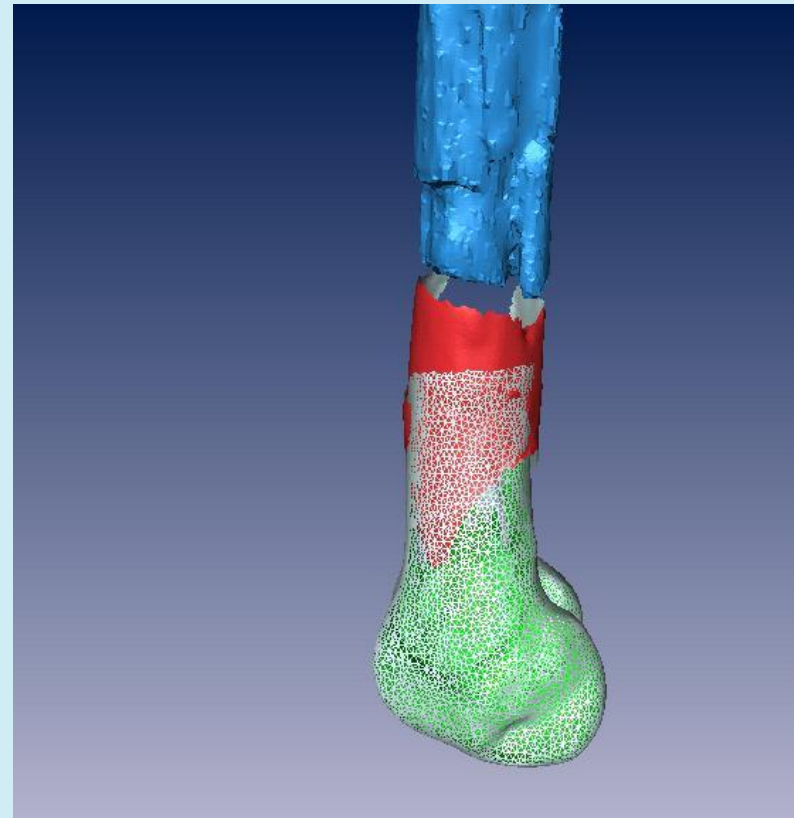
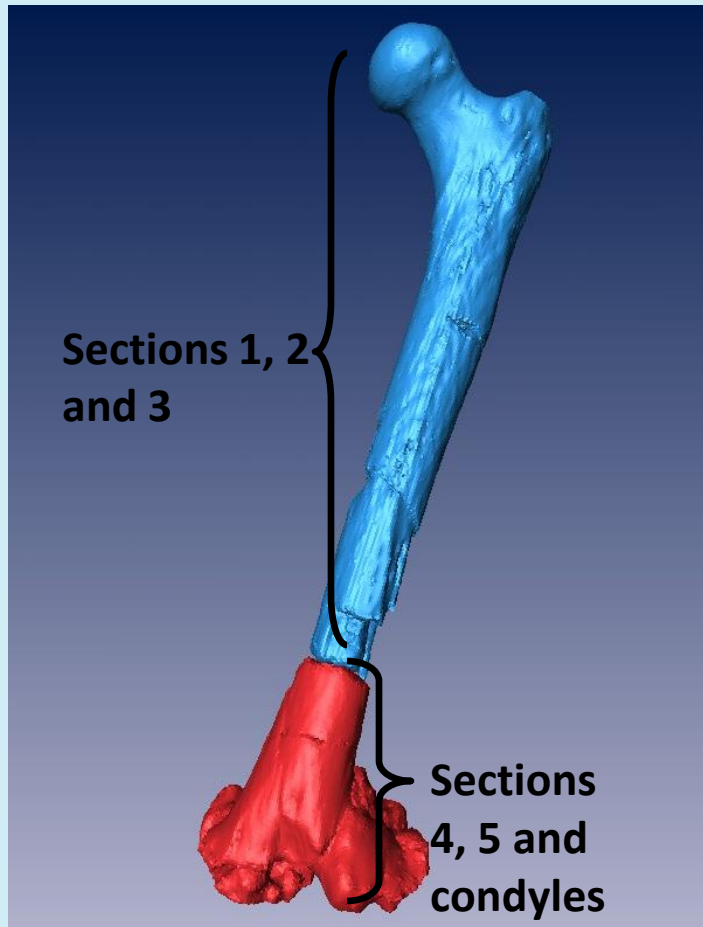
- **Extrapolation of missing bone segments**



Fragmentary Bone Reconstruction (Traditional By Hand)

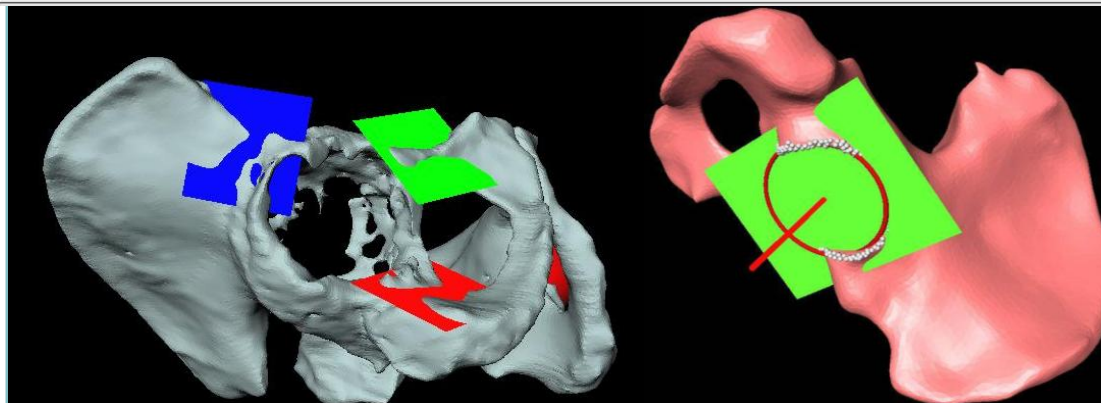
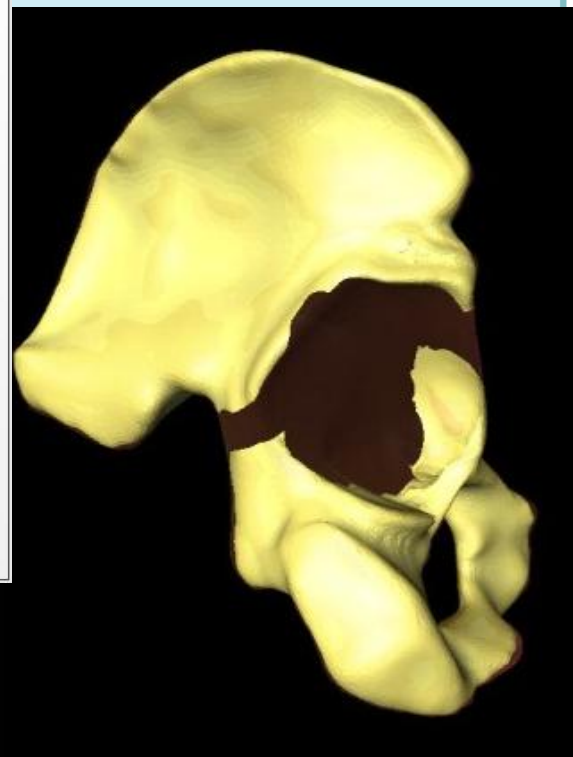
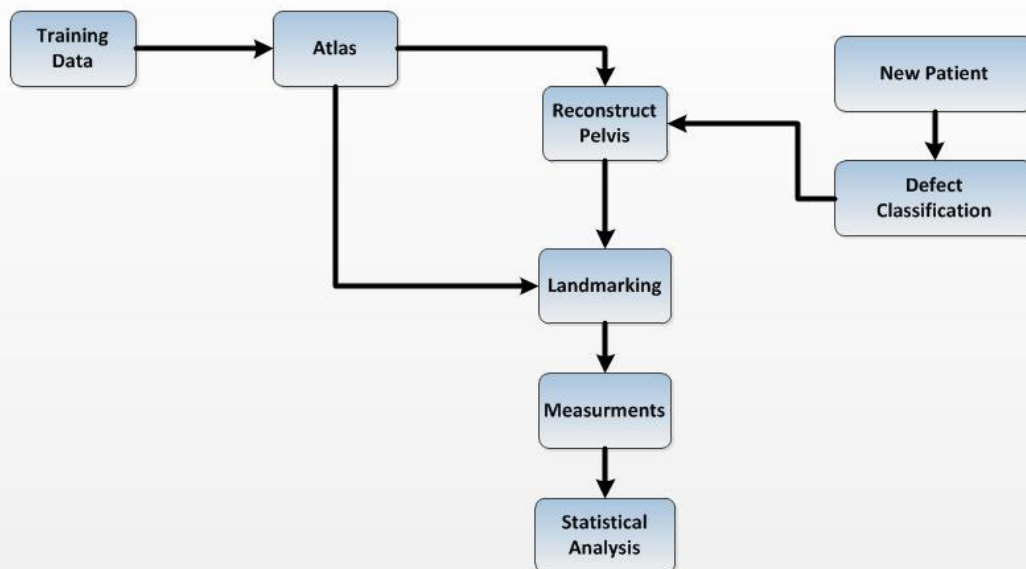


Reconstruction : Conjoinable Pieces

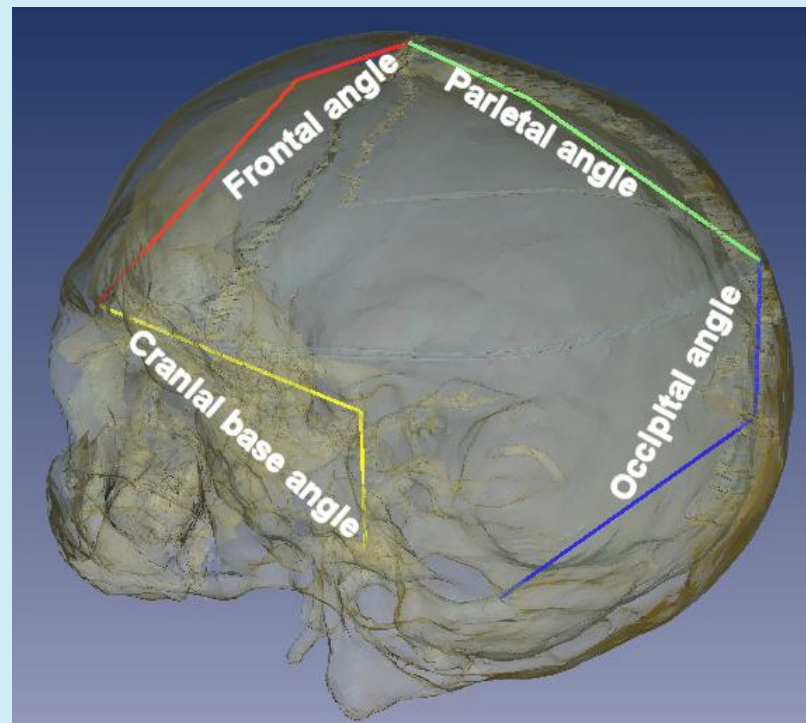
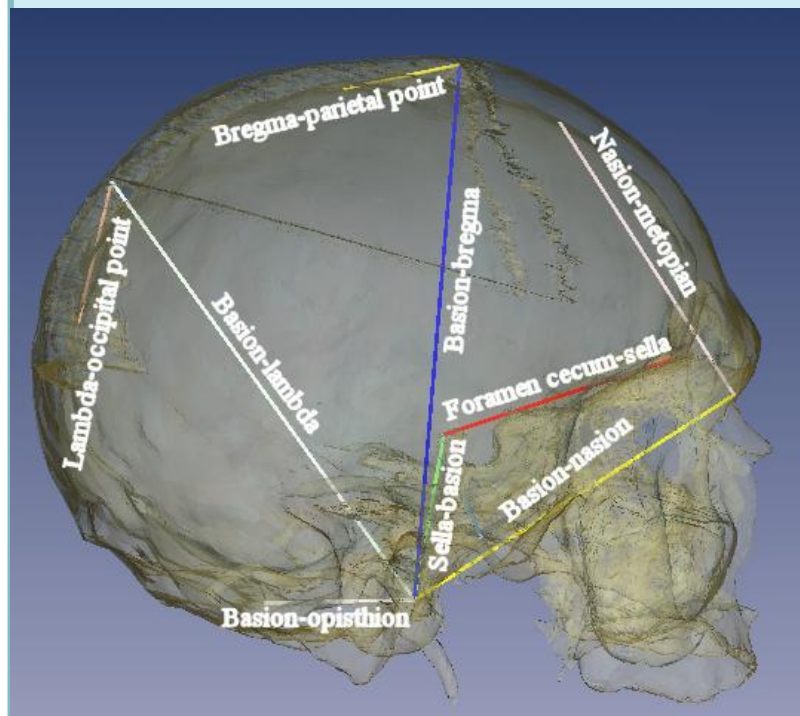


From Sylvester, Merkl and Mahfouz (2008).

Pelvis Reconstruction



Automatic Measurements (Skull)



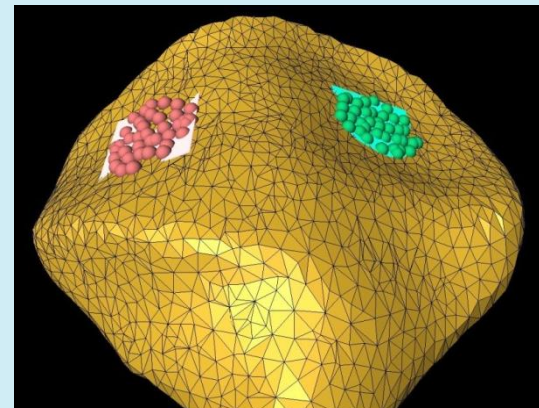
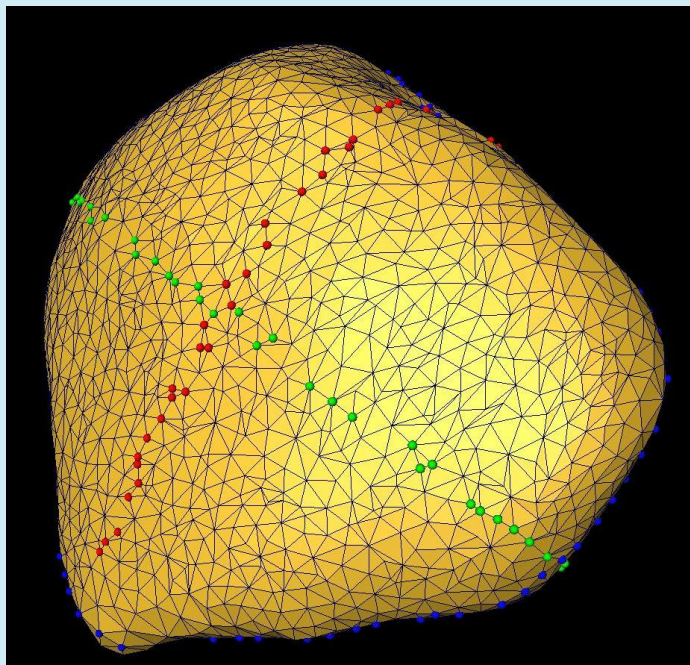
Skull Sexing 98% Using 11 Features

From Shirley, Abdel Fatah, Jantz and Mahfouz (2011).

Thickness Measurements (Skull)

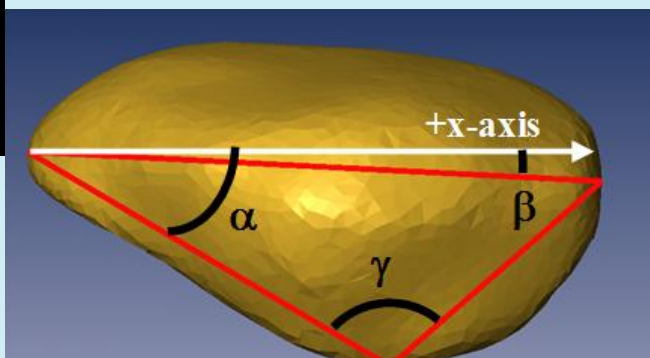


Automated Measurements (Patella)



Posterior Facet Angle

**Circumference Moment
Measurements Around
3 Coordinate Axes**



2D In-plane Measurements

Patella Sexing

Testing results of confusion matrix using a neural network trained on the full 45 features (93.51% correctly classified)

Actual	Predicted		
	Females	Males	Total
Female	28	3	31
Male	2	44	46
Total	30	47	77

From Mahfouz, Badawi, Merkl, Abdel Fatah, Pritchard, Kesler, Moore, Jantz and Jantz (2007).

Cited Scientific References

- Mahfouz, M.R.; Badawi, A.M.; Merkl, B.C.; Abdel Fatah, E.E.; Pritchard, E.; Kesler, K.; Moore, M.K.; Jantz, R.L.; Jantz, L.M. Patella Sex Determination by 3D Statistical Shape Models and Nonlinear Classifiers. *Forensic Science International* 2007, 173(2), 161-170.
- Moore, M.K.; Mahfouz, M.R.; Abdel Fatah, E.E.; Badawi, A.M. Comparison of Dry and In Vivo Bone Densities from CT Images using Fuzzy Logic and Neural Networks. *Computer Methods in Biomechanics and Biomedical Engineering, 7th International Symposium, Cote De Azure, France, 2006.*
- Shirley, N.R.; Abdel Fatah, E.E.; Jantz, R.L.; Mahfouz, M.R. Improving Sex Estimation from the Human Cranium Using 3D CT Scans. *American Academy of Forensic Sciences, 63rd Annual Scientific Meeting, Chicago, IL, 2011.*
- Sylvester, A.D.; Merkl, B.C.; Mahfouz, M.R. Reconstructing the AL 288-1 Femur Using Three-Dimensional Computer Models. *Journal of Human Evolution* 2008, 55, 665-671.

Questions?

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