

Technology Transition Workshop | *Mohamed R. Mahfouz, Ph.D.*

History and Application of Computed Tomography (CT) Images

Outline

- **Why 3D?**
- **CT Principles**
- **Calibration**
- **Modeling**
- **Applications**

Why 3D?

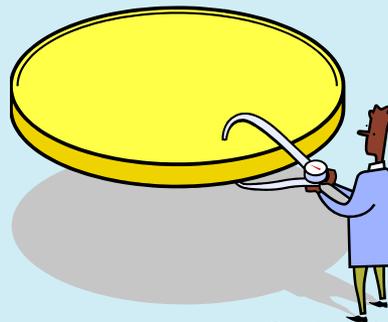
Conventional Methods

- X-Ray



© Microsoft

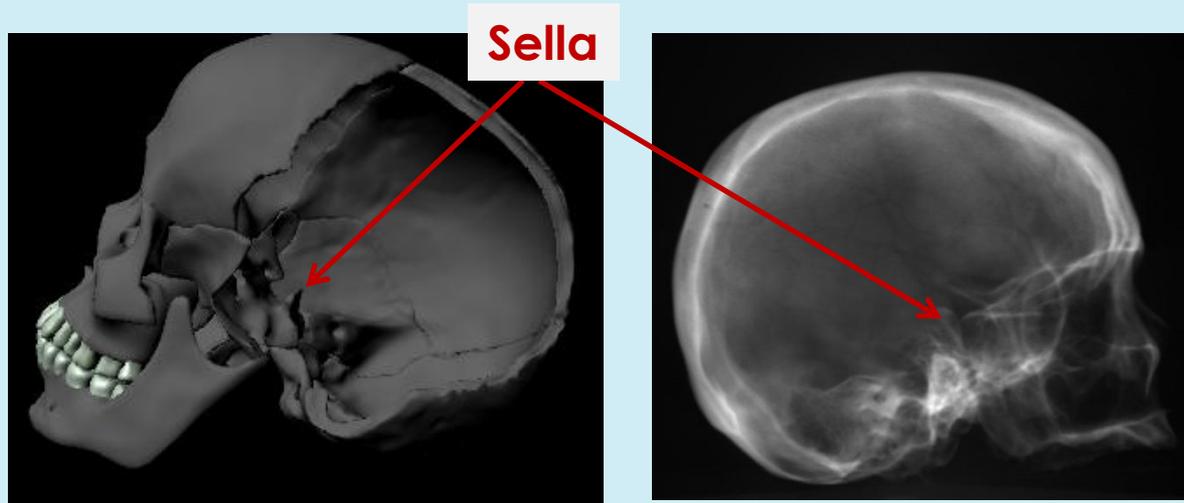
- Calipers



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X-Ray

- 2D Projection of 3D Anatomy
 - Dense object can shadow structure behind it
 - No depth perception
 - Projection change by rotating object relative to imaging plane
 - Limited soft tissue information

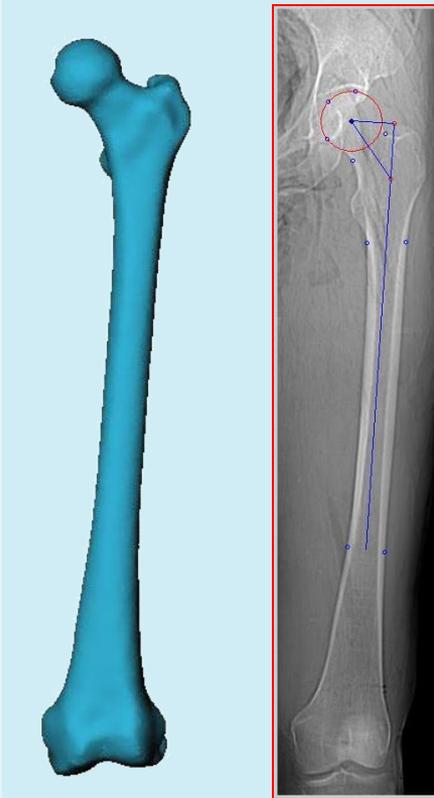


X-Ray Accuracy

Female Case

X-Ray Proximal Angle = 142.78

True 3D proximal angle = 130.84



Male Case

X-Ray Proximal Angle = 140.16

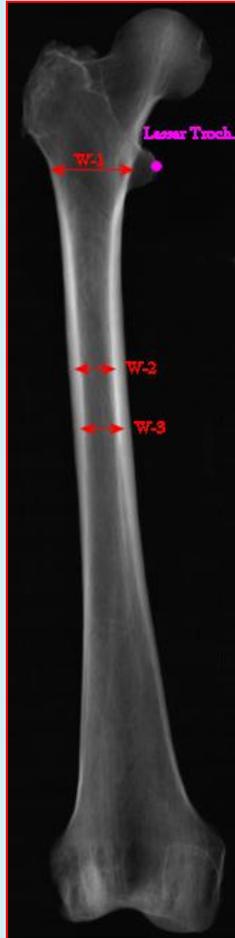
True 3D proximal angle = 127.62



Effect Of Rotation on X-Ray



Effect Of Rotation on X-Ray



2-D Measurements

	W-1	W-2	W-3
μ	7.90%	4.62%	2.25%
σ	5.90%	3.01%	2.51%

Percentage Error in 2-D Measurements
Due to 12° External Rotation

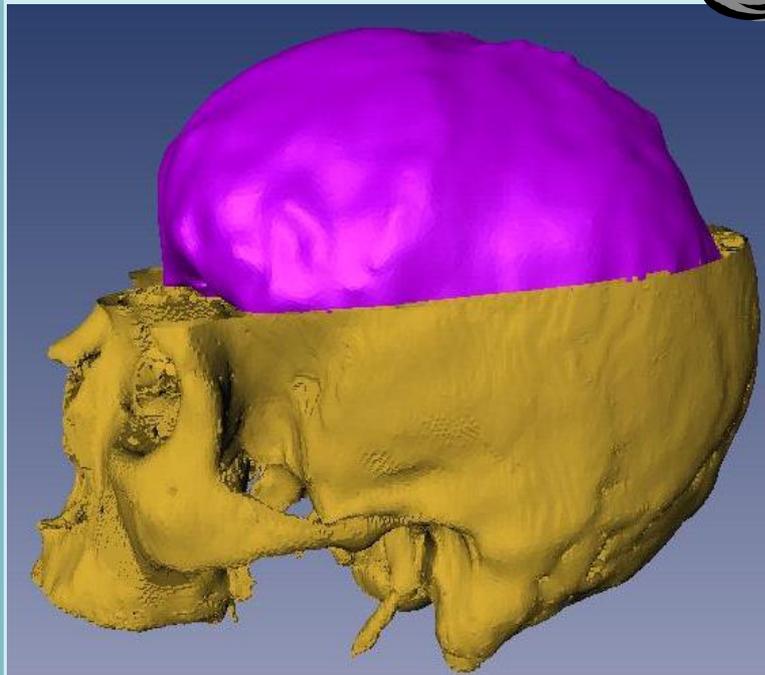
	W-1	W-2	W-3
μ	5.84%	3.83%	1.41%
σ	6.23%	1.73%	1.75%

Percentage Error in 2-D Measurements
Due to 10° Internal Rotation

Calipers

- **Intra- and inter-observer error**
- **Can be only used for geodesic measurements**
- **Limited access to anatomical features**
 - **Finding internal landmarks (autopsy)**
 - **Limited number of landmarks**
- **Time consuming**

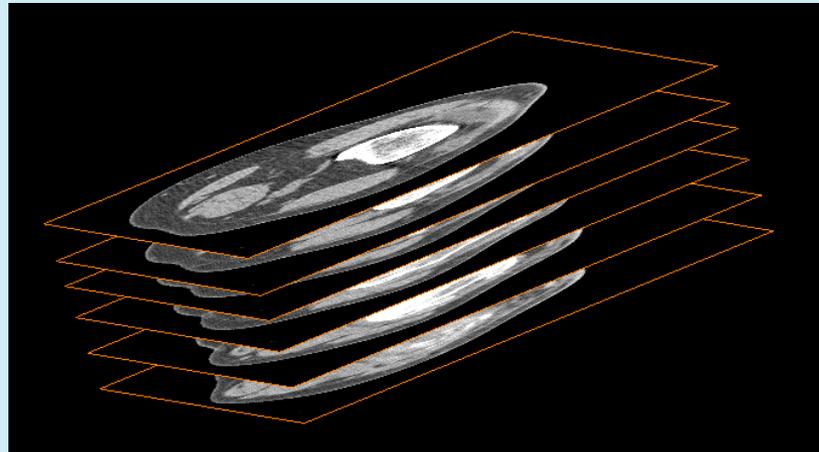
Calipers



How To Measure Volume???

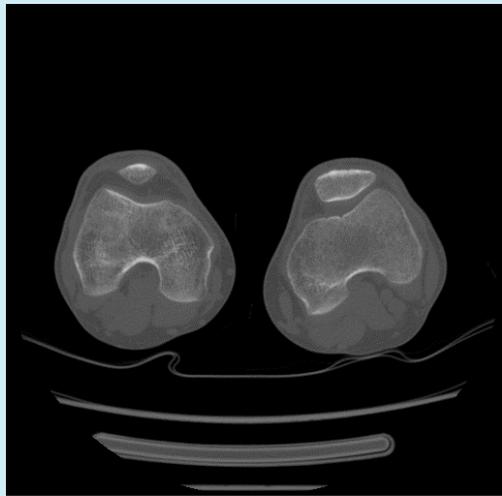
CT

- **What's a CT?**
 - **X-Ray device capable of imaging cross sections of object**
 - **Create stack of images; each represents slice from object**
 - **Images stacks can be arranged in 3D to create volume**



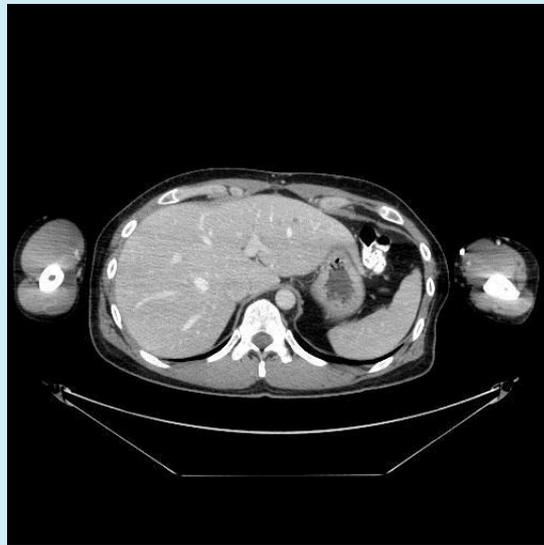
CT Applications

- **Wide range of applications in both soft tissue and bones**



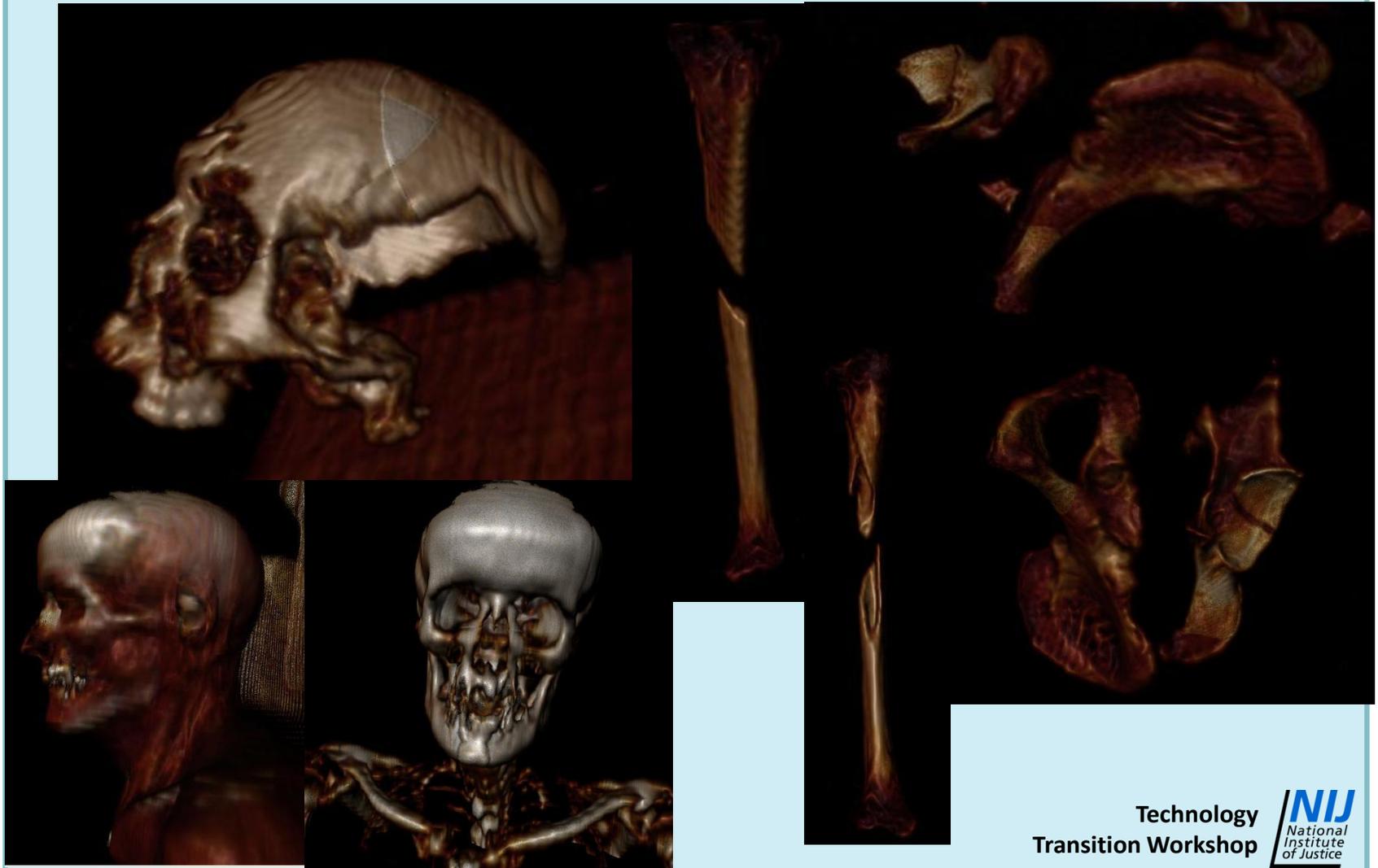
Knee

Lumbar



Hip

CT Applications



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CT History

- **Computed tomography (CT) became the historically first tomographic modality entirely based on digital reconstruction of images**
- **Medical image reconstruction refers to the reconstruction of cross sectional or volume data from the projection data at various angles**
- **Introduced by Hounsfield and Cormack**
- **Nobel Price 1979 (Physiology or Medicine)**

Sir Godfrey Newbold Hounsfield
1919-2004

Nobel Price for Medicine : 1979



© Vanderbilt University Medical Center

Prof. Allan McLeod Cormack
1924-1998

Nobel Price for Medicine : 1979

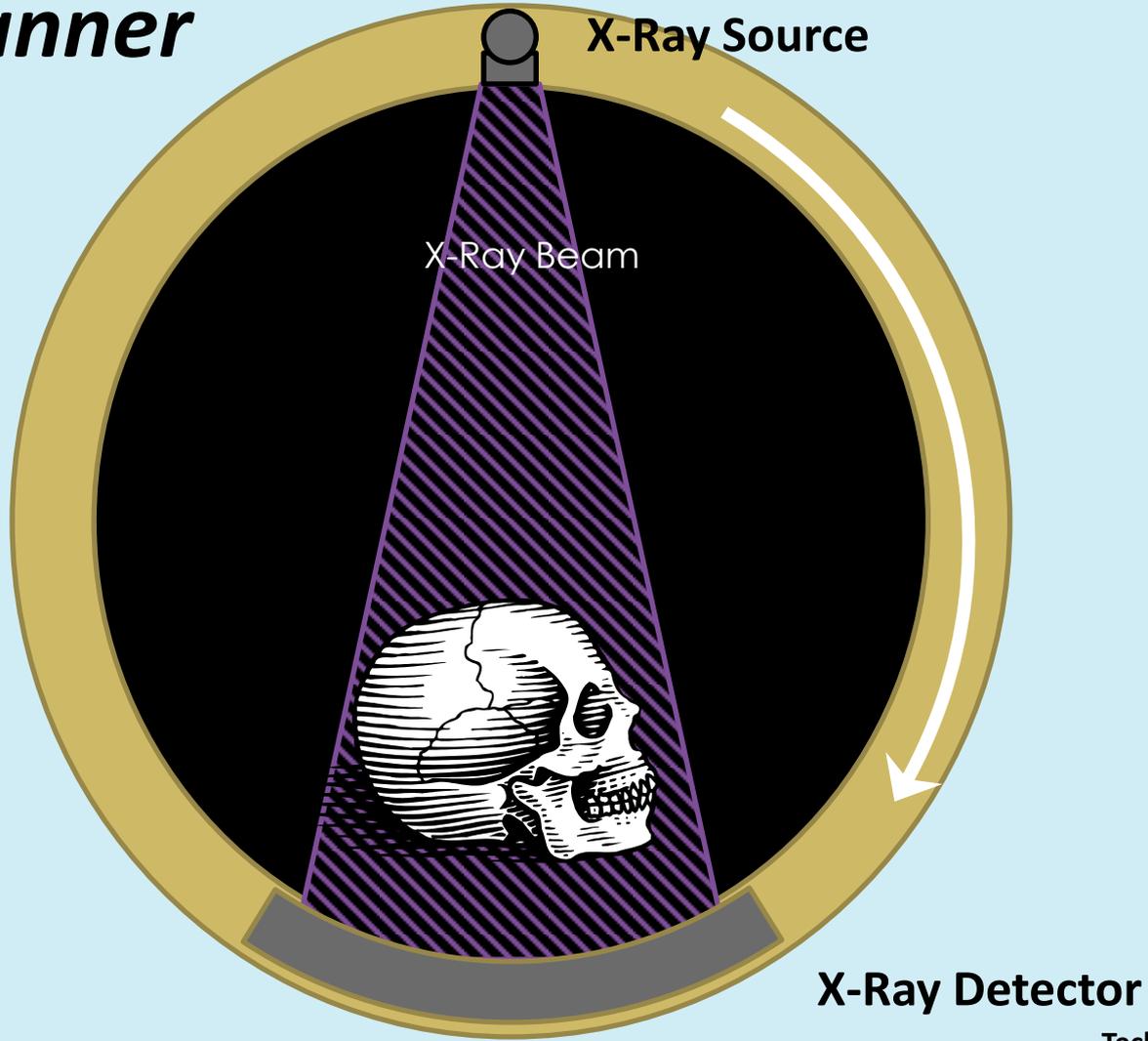


Courtesy of Freebase.com

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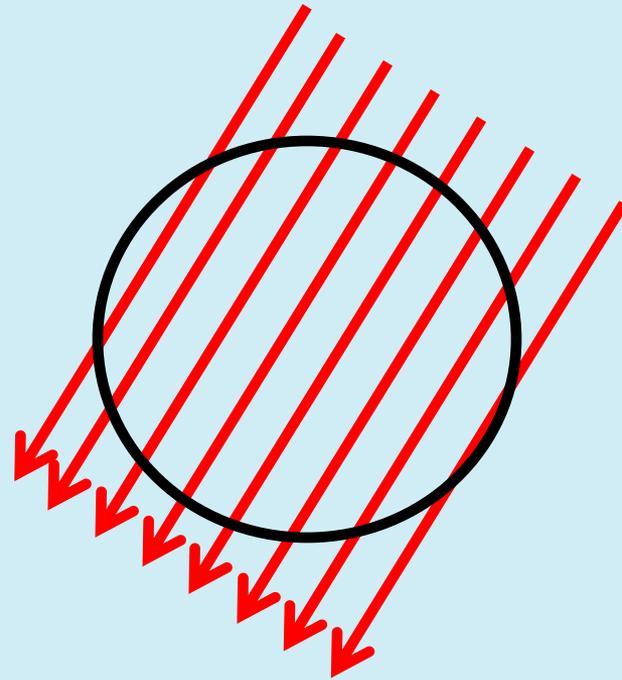
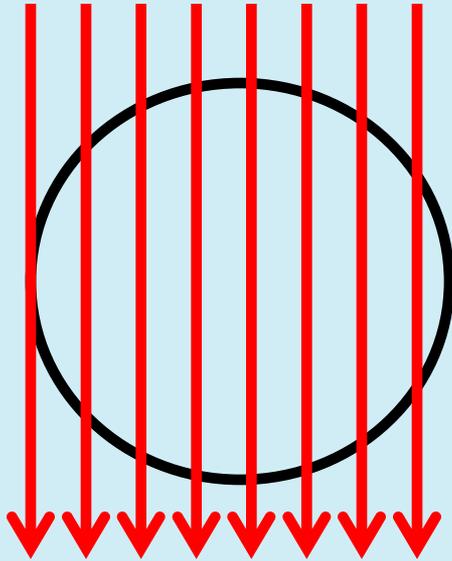
CT Scanner



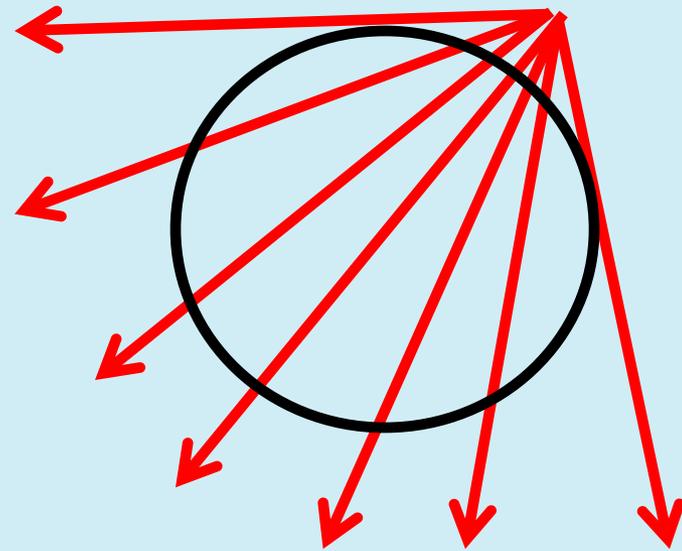
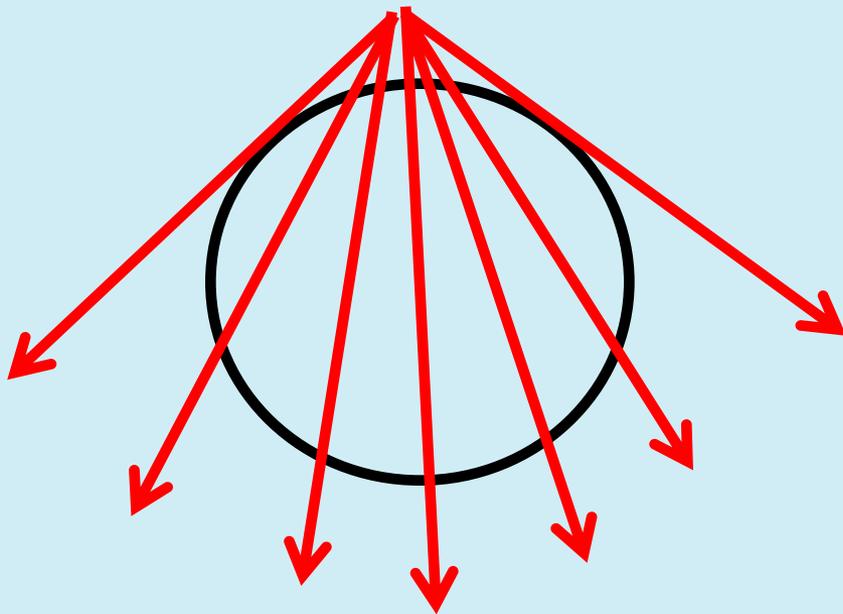
Basic Idea

- **2D views (projections) at all angles around the patient**
 - **Rotating source and detector**
 - **Sample attenuation at each detector for each angle**
 - **Generate projections**
 - **Different beam geometry**
 - **Parallel**
 - **Fan**
 - **Cone**

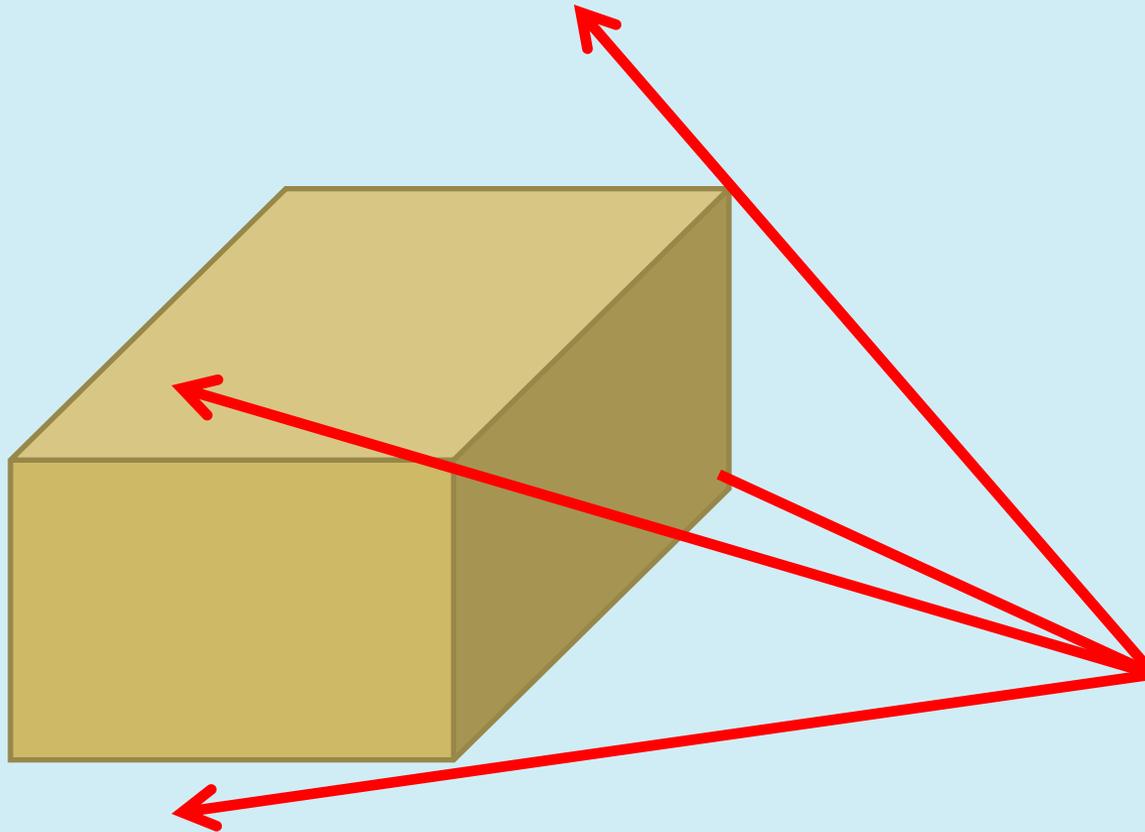
Parallel Beam



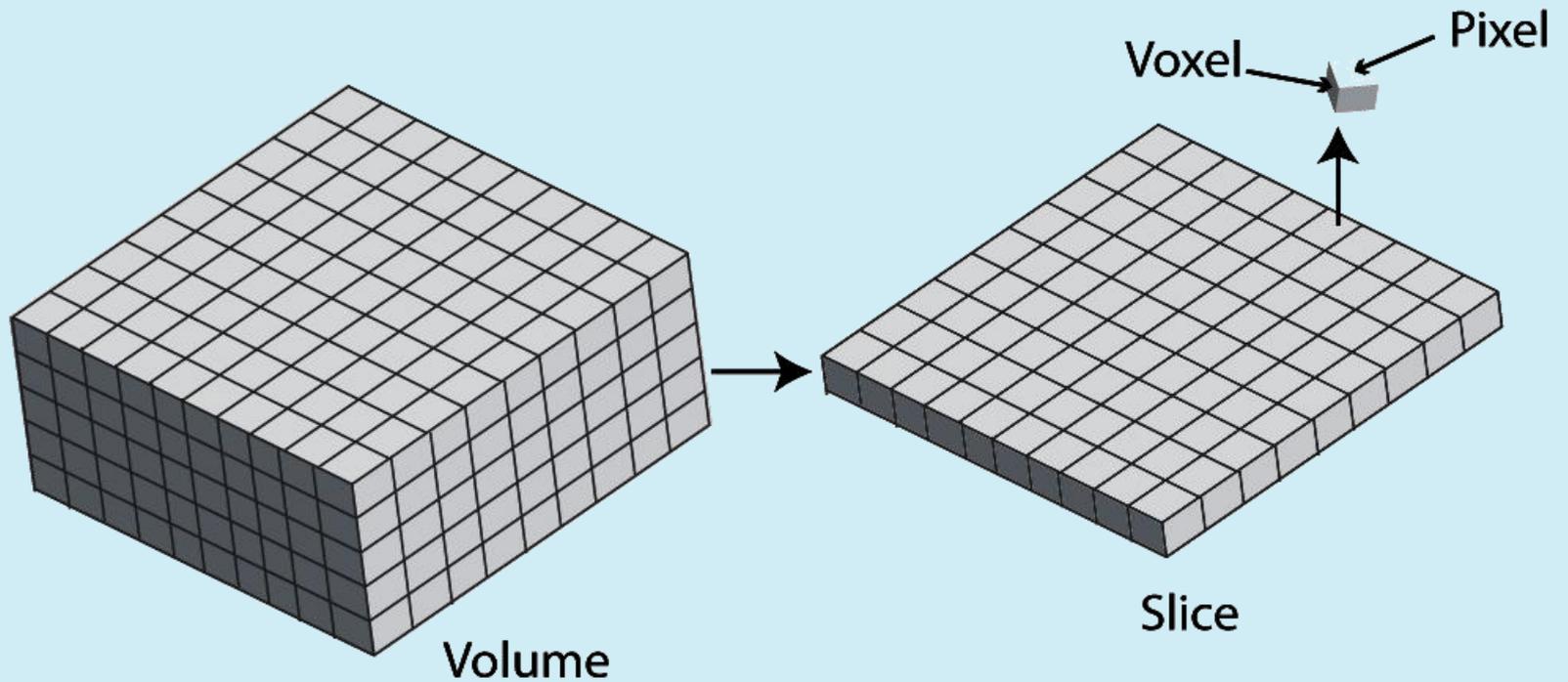
Fan Beam



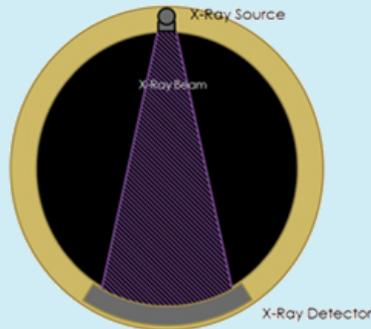
Cone Beam



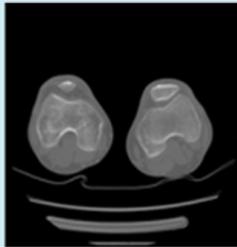
Pixel vs Voxel



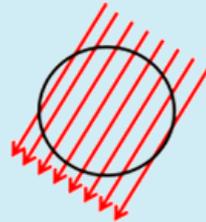
CT Reconstruction



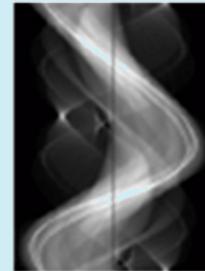
Attenuation Data from rotating source and detector around object



Reconstructed Image



Reconstruction Routine



Sinogram: a line for every angle

CT Number

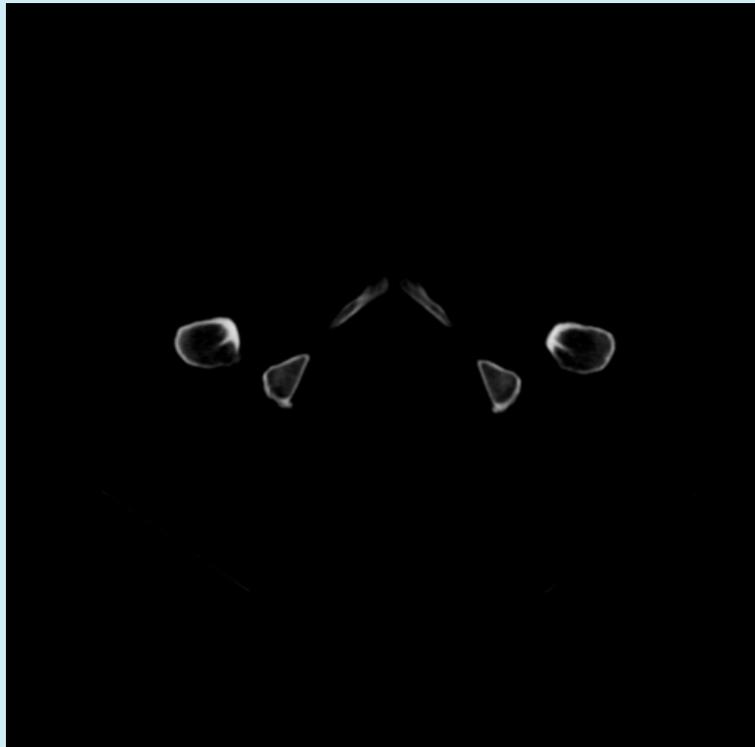
- **Images:**
 - **Size generally 512*512**
 - **Linear attenuation coefficient measured between tube and detector**
 - **Attenuation coefficient measure: how x-ray absorbed with material**
 - **Values in Hounsfield Units (HU)**

$$\text{CT number (HU)} = \frac{\mu - \mu_{H_2O}}{\mu_{H_2O}} * 1000$$

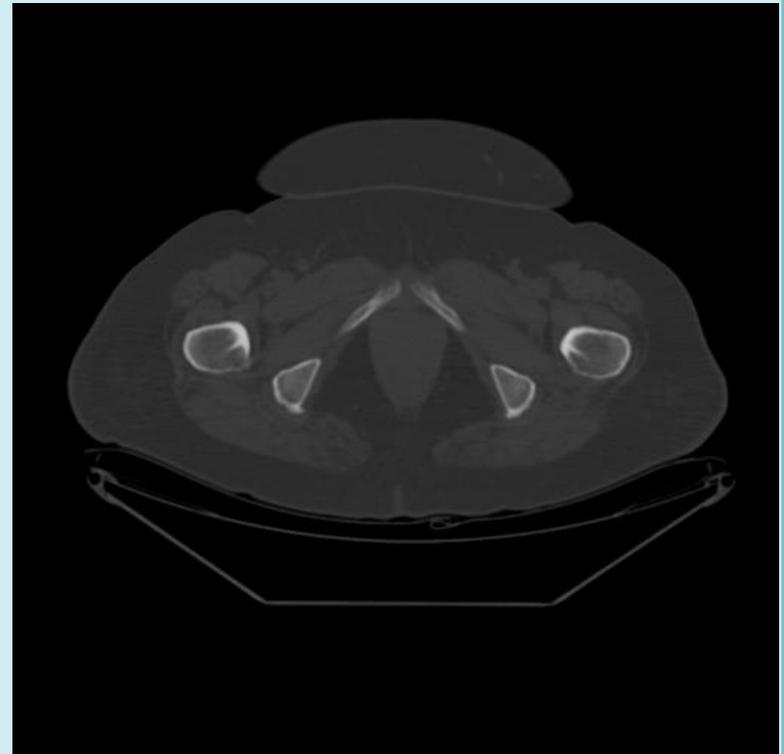
CT Number Window

- **Due to large dynamic range, windowing is used to view images**
- **The windowing affects both brightness and contrast**
- **Window is defined by Window Level (WL) and Window Width (WW)**
 - **WL is CT number of the mid gray**
 - **WW is number of HU from black to white**

CT Number Window



WL: 752
WW: 2639



WL: 899
WW: 1531

CT Parameters

- **Acquisition parameters**
 - Determine production of scan data set
- **Reconstruction parameters**
 - Determine presentation of the data

Acquisition Parameters

- **Tube potential**
 - Voltage between cathode and anode
 - Measured in KeV
 - Higher potential accelerates electrons and thus increase x-ray energy
- **Tube current**
 - Current flowing through cathode
 - Measured in mA
 - Larger current increases number of electrons and thus increases beam intensity

Acquisition Parameters (Continued)

- **Scan time**
 - Time taken for tube and detectors to perform complete rotation
 - Longer scan time increases total x-ray count
- **Collimation\slice thickness**
 - Width of CT slice along z-axis
- **Beam filtration**
 - Different beam shaping filter, optimized for different examinations

Reconstruction Parameters

- **Field of view**
 - Size of image in X and Y directions
- **Reconstruction matrix**
 - Usually 512*512
- **Reconstruction filter**
 - Different filters available from smooth (soft tissue) to sharp (bone)

CT Generations

- **1st generation**
 - **Single detector**
 - **Translate – rotate acquisition**
 - **Translate across patient**
 - **Rotates around patient**
 - **Very Slow**
 - **Minutes per slice**

CT Generations (Continued)

- **2nd Generation**
 - **Narrow fan beam (10 degree)**
 - **Multiple detectors**
 - **Rotation and translation**
 - **Slow**
 - **20 seconds per slice**

CT Generations (Continued)

- **3rd Generation**
 - **Wide fan beam**
 - **Multiple detectors (500-1000)**
 - **Rotation only**
 - **Multiple angle acquisition at each position**
 - **Faster**
 - **0.5 second per rotation**

CT Generations (Continued)

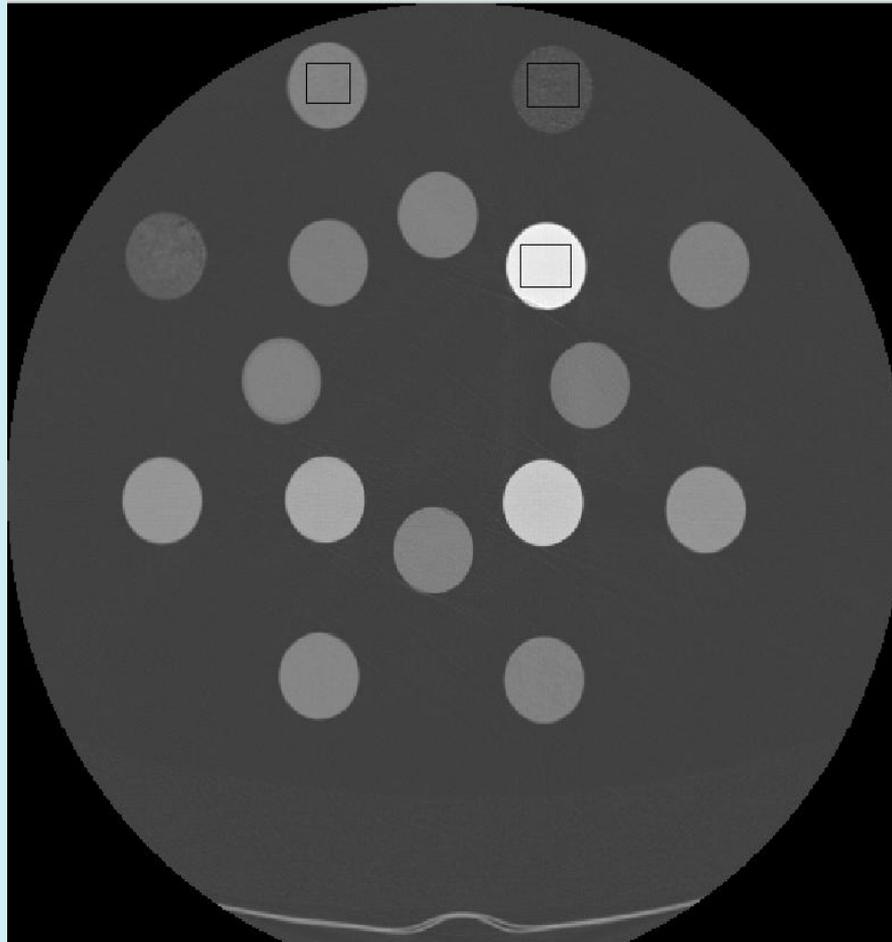
- **4th Generation**
 - Fan beam
 - Static detectors all around gantry
 - Only tube rotates

Calibration Phantom

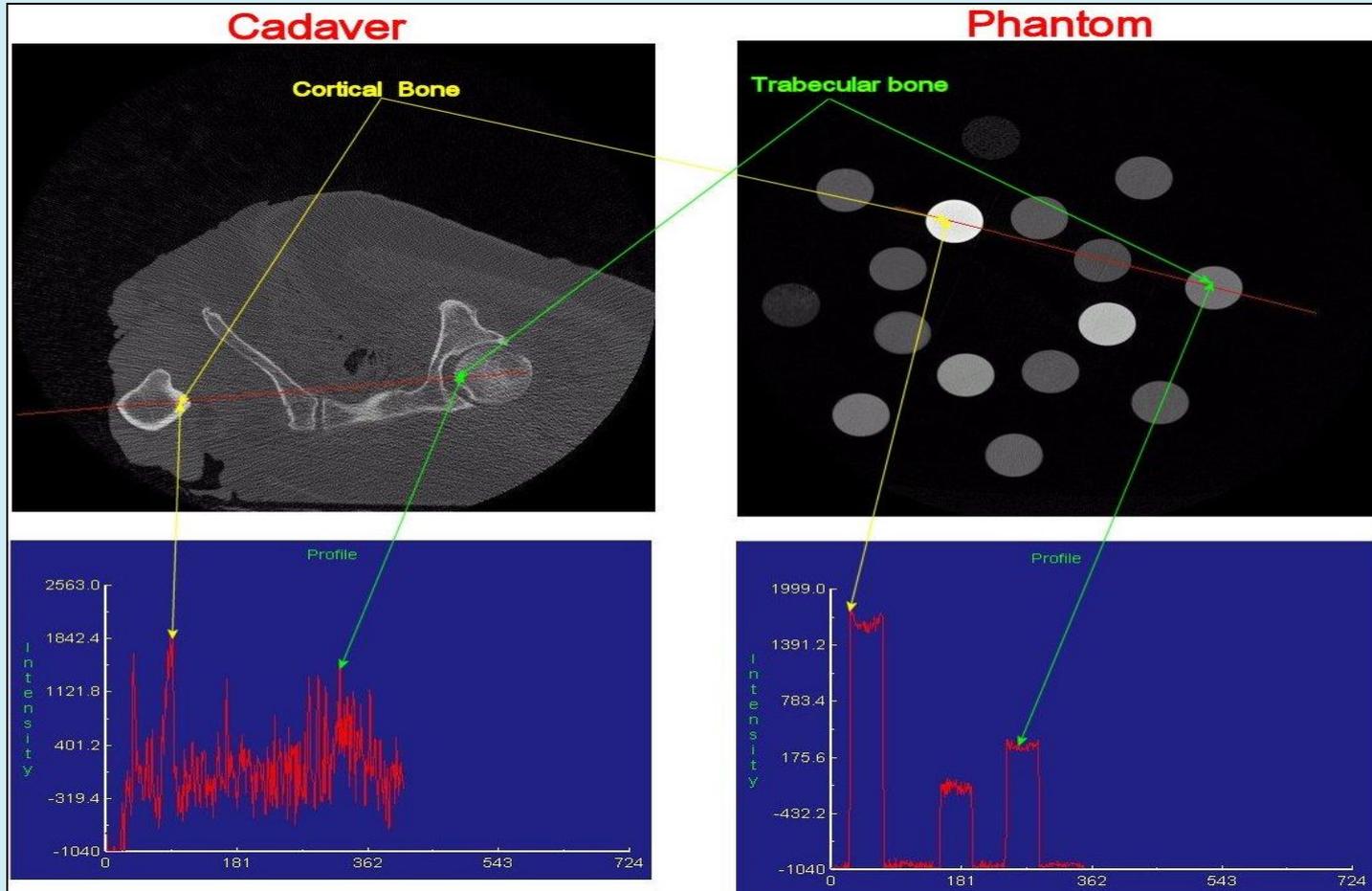
- Has similar properties to human tissue
- Used in procedures for measurement of absorption of radiation
- Used for calculating bone density



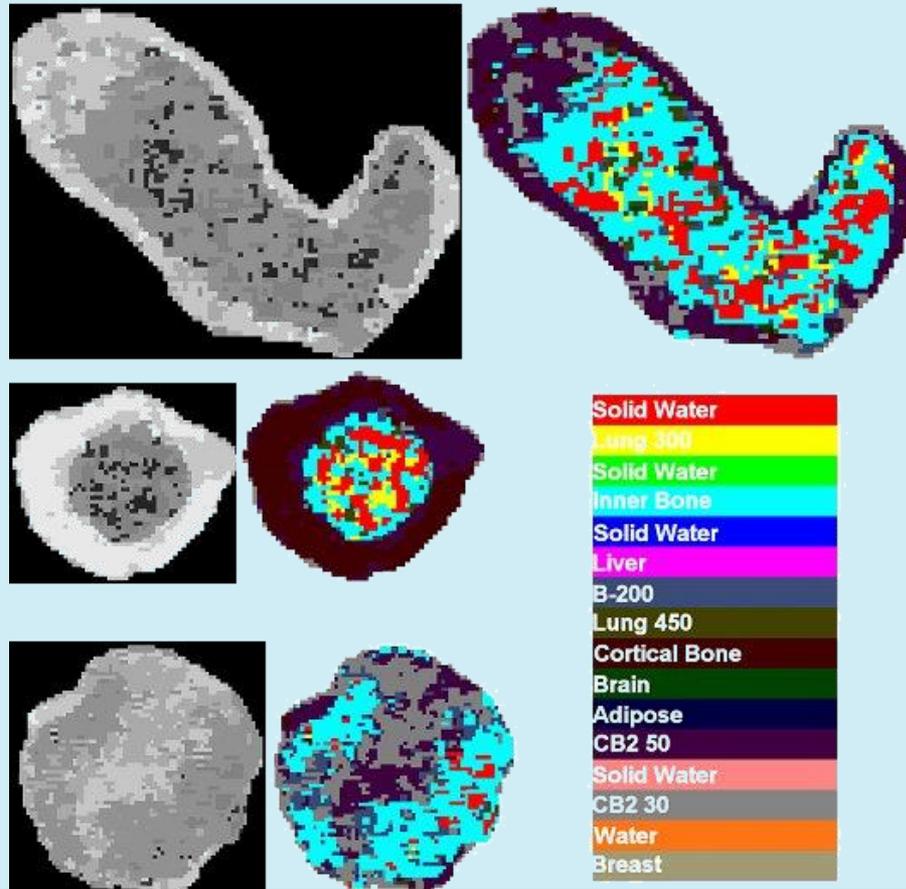
CT Image of Phantom



Density Mapping



Density Mapping



Density and Color Map for Different Parts in Proximal Femur

From Moore, Mahfouz, Abdel Fatah and Badawi (2006).

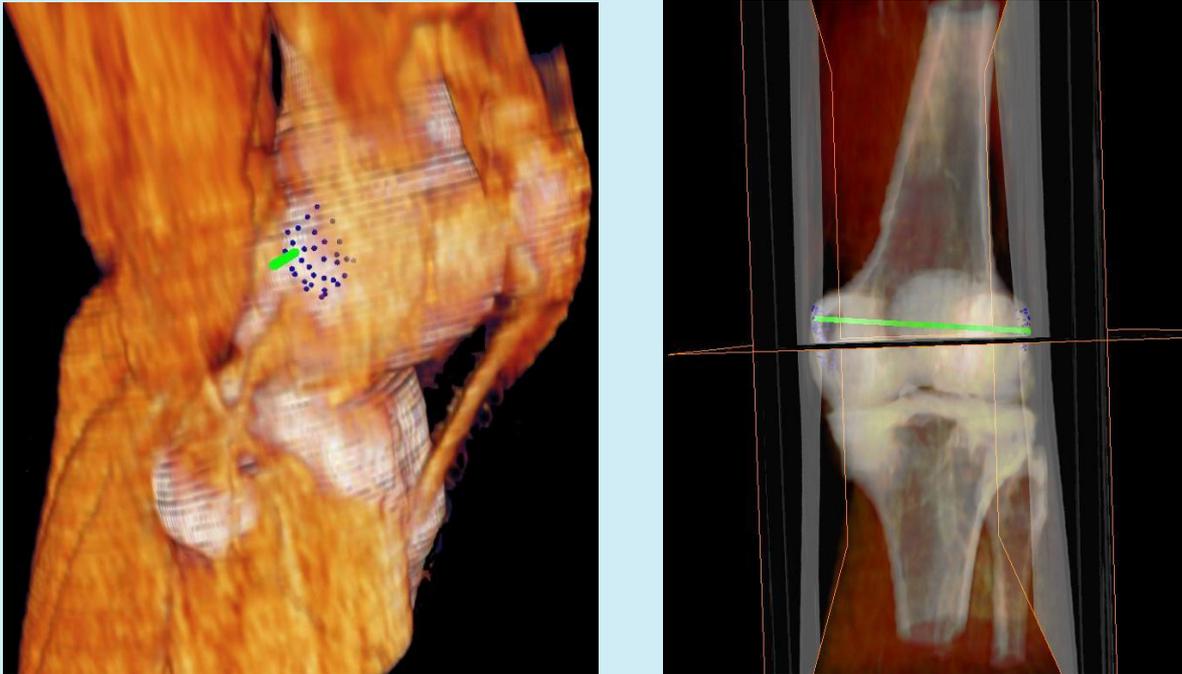
Modeling

Two Methods:

- 1. Directly find landmarks or perform measurements on CT slices**
- 2. Generation of 3D surface model by segmenting object of interest, then perform measurements on the segmented model**

Modeling Directly from CT Slices

- Features can fall between slices

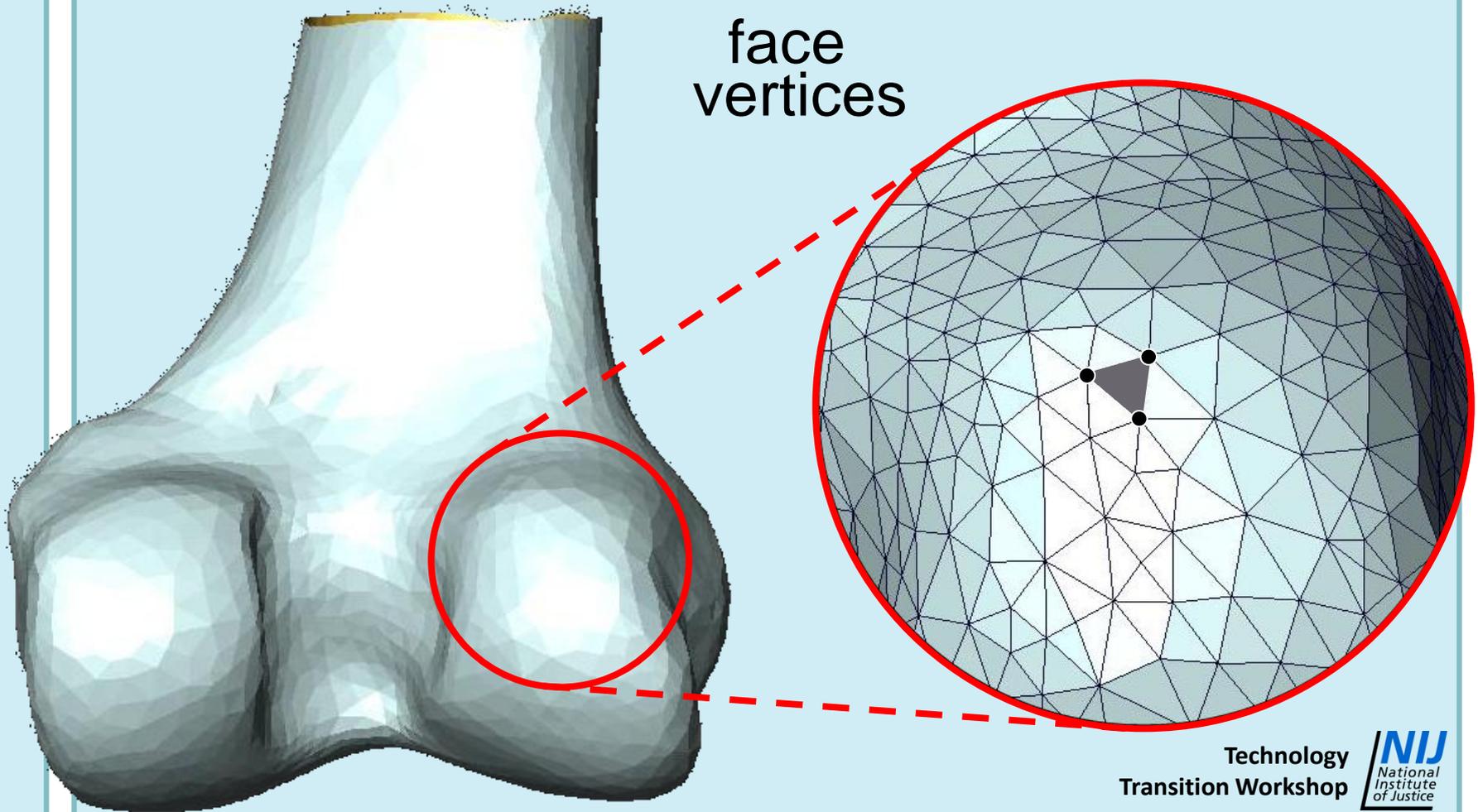


Example: Epicondylar Axis in Femur

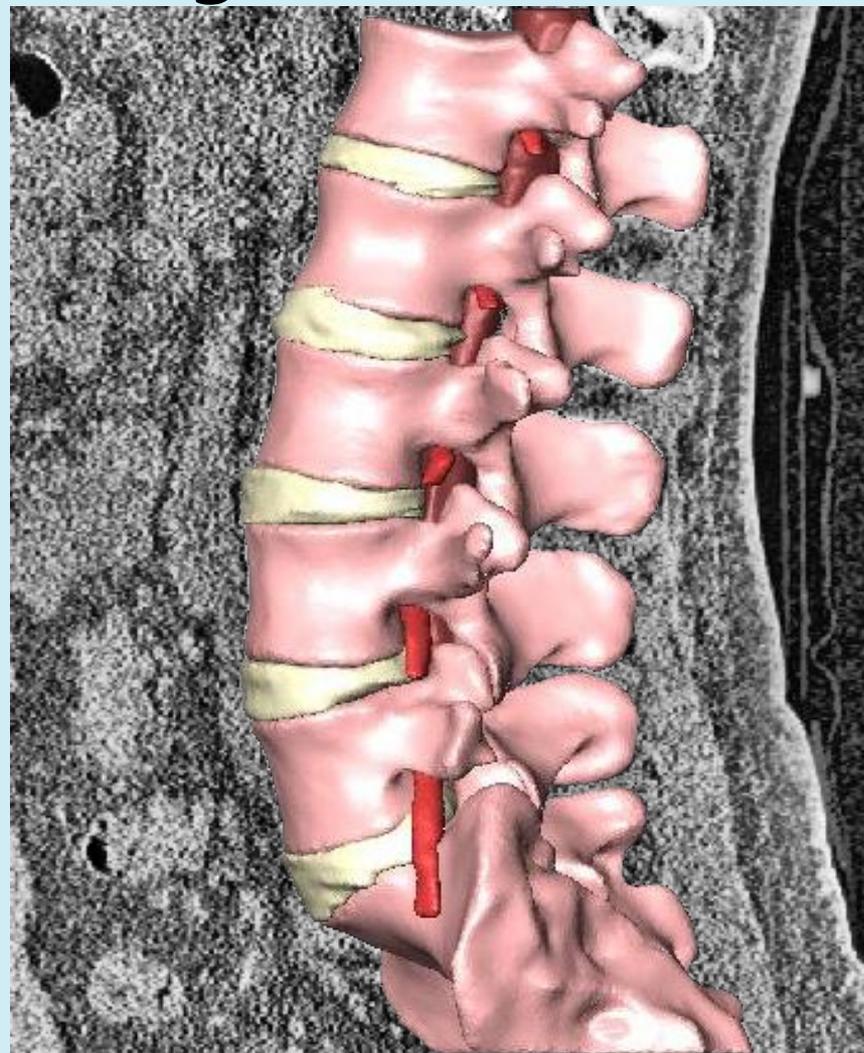
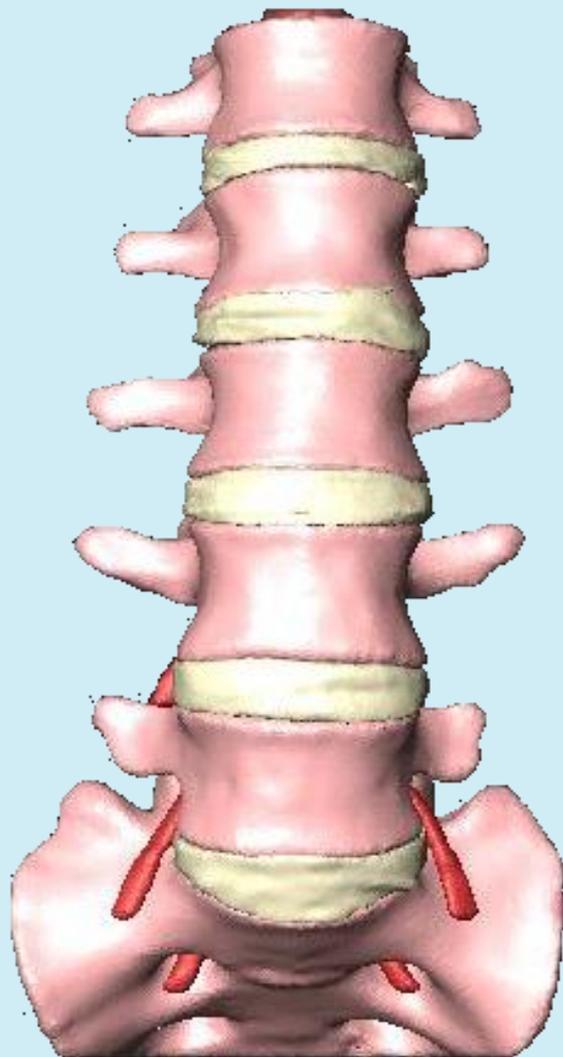
Modeling Using 3D Models

- **Segmentation**
- **Statistical atlases**
- **Reconstructing missing data**
- **Measurements and landmarking**
- **Statistical analysis**

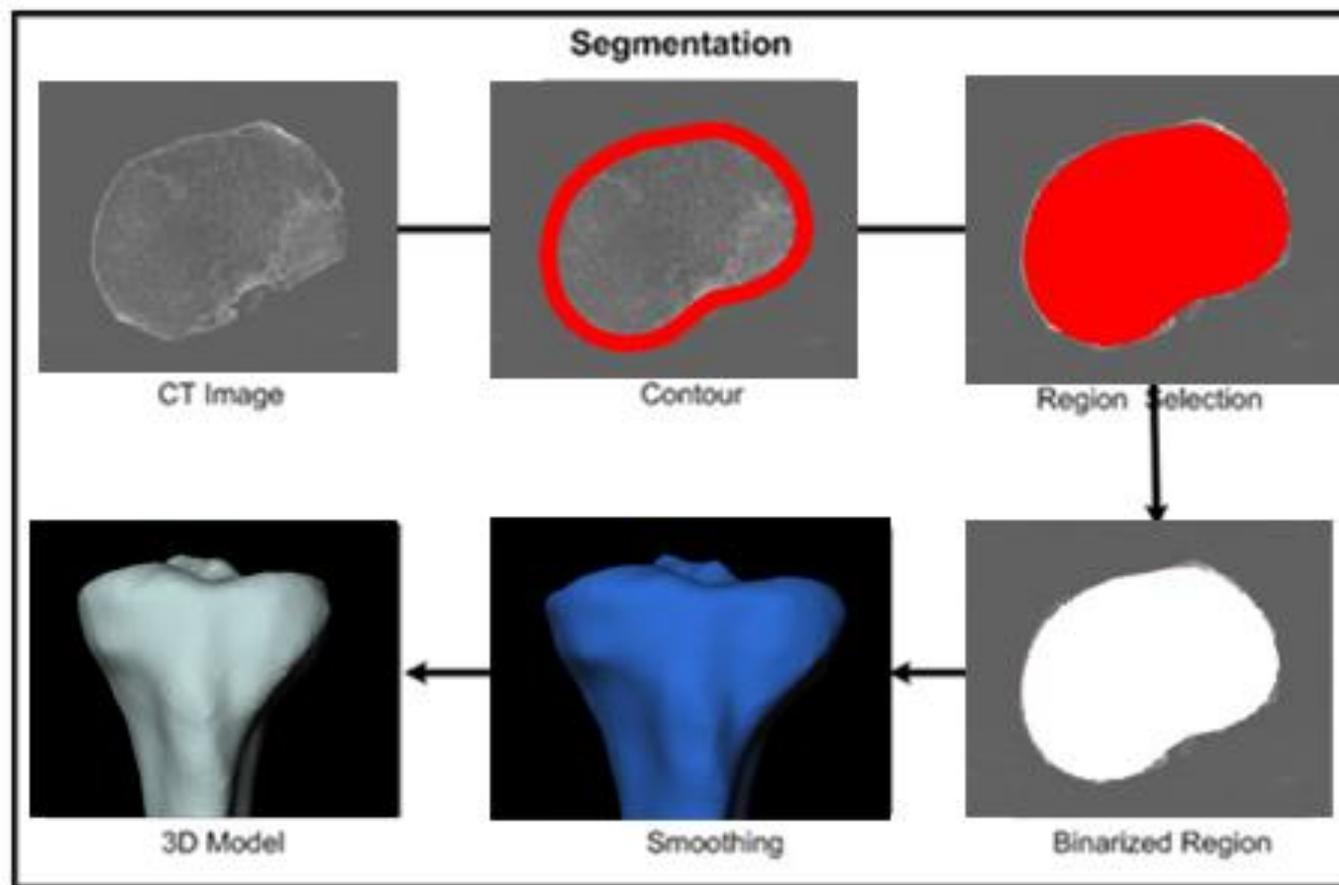
What is a 3D Model?



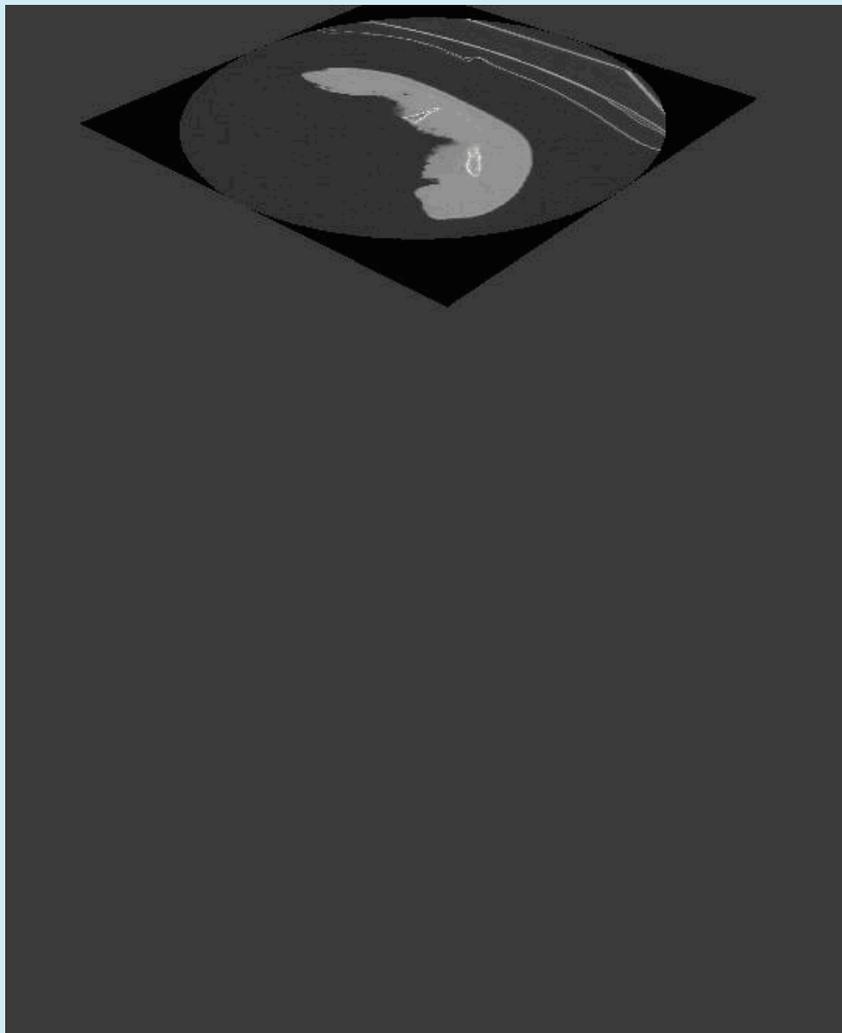
3D Models vs 2D Images



Model Segmentation



Model Segmentation

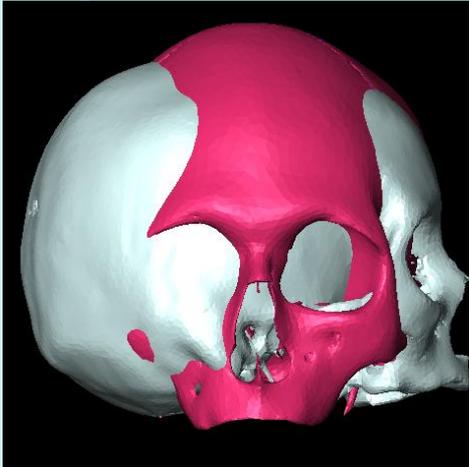


Statistical Bone Atlas

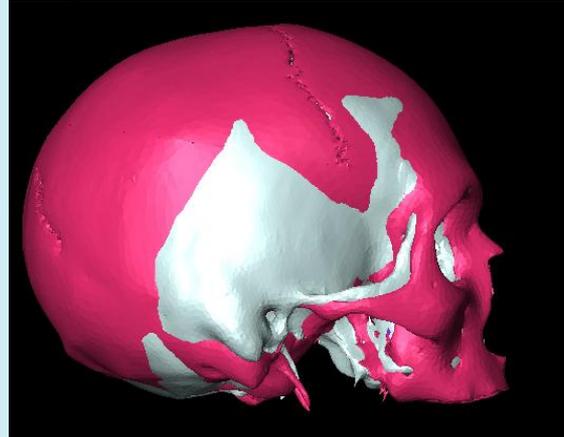
- **Generate surface mesh models built from computed tomography data**
 - **New models are converted to a normalized mesh**
 - **Models then represented with principal components that govern bone shape**
- **Statistical variation of morphology can be computed for a population of bones**
- **“Average” bone model computed from bones in the atlas**

Statistical Atlas

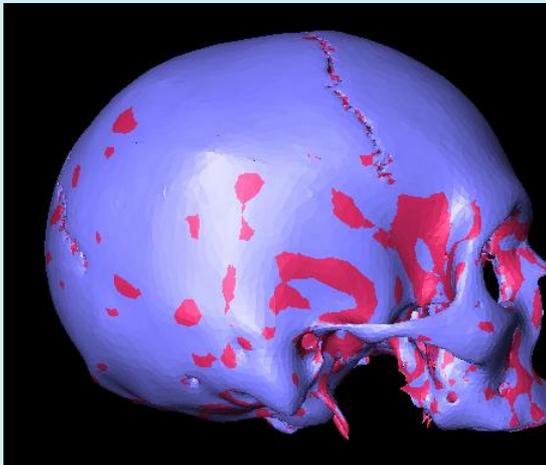
Align bone centroids



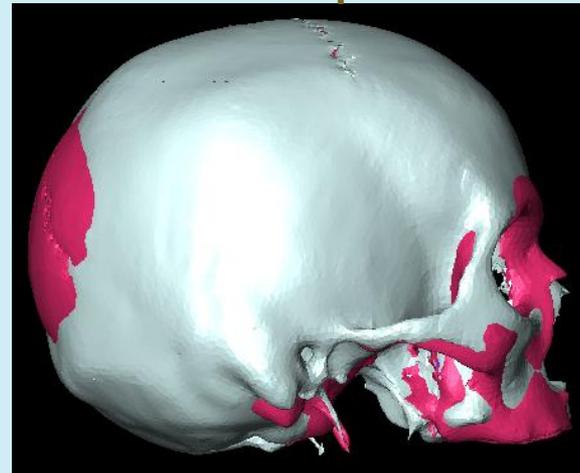
Perform Rigid Iterative Closest Point (ICP)



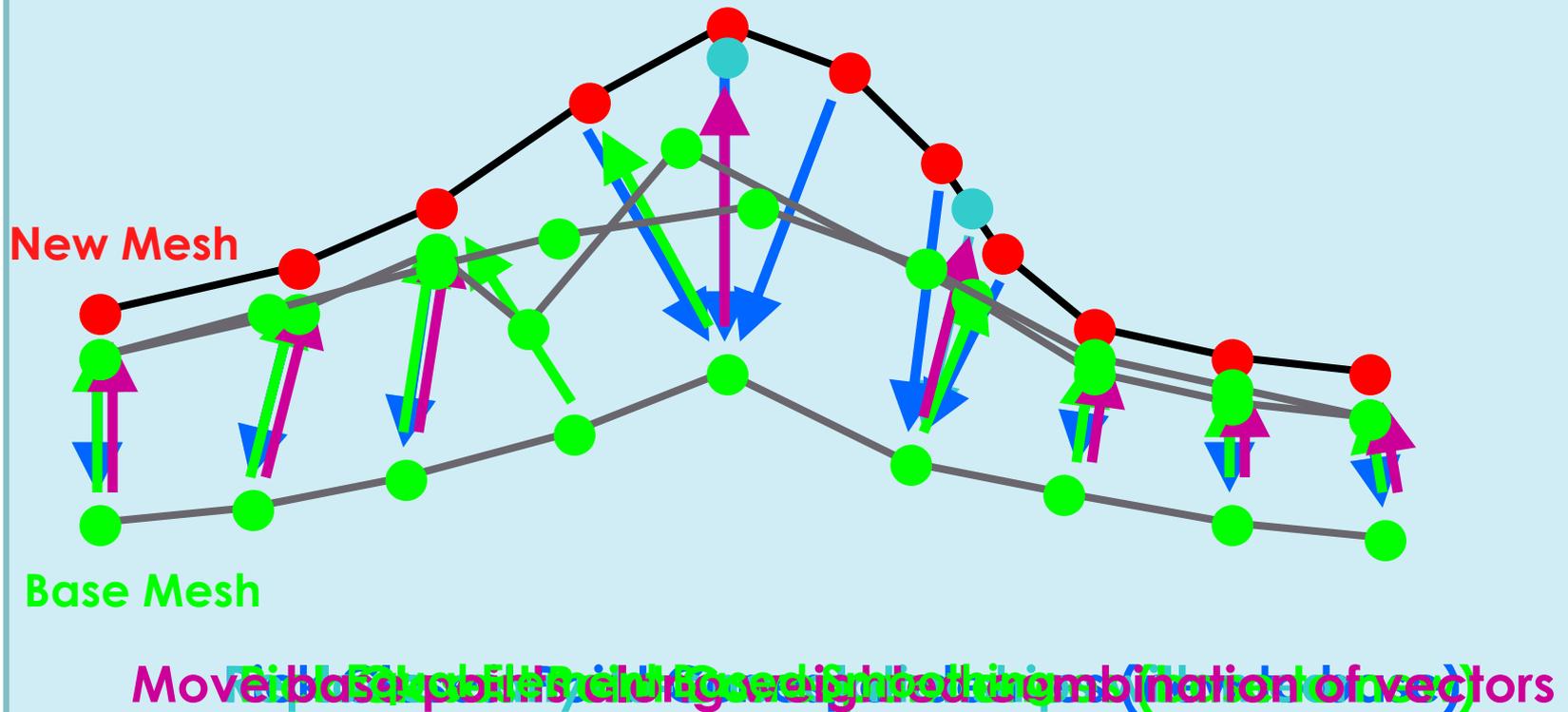
Free Form Transformation



Surface Correspondence



Surface Correspondence



Feature Extraction Techniques

*Statistical
Shape Model*

**Principal
Components
(PCA)**

(Global)

*Specific
Landmarks*

Measurements

(Local)

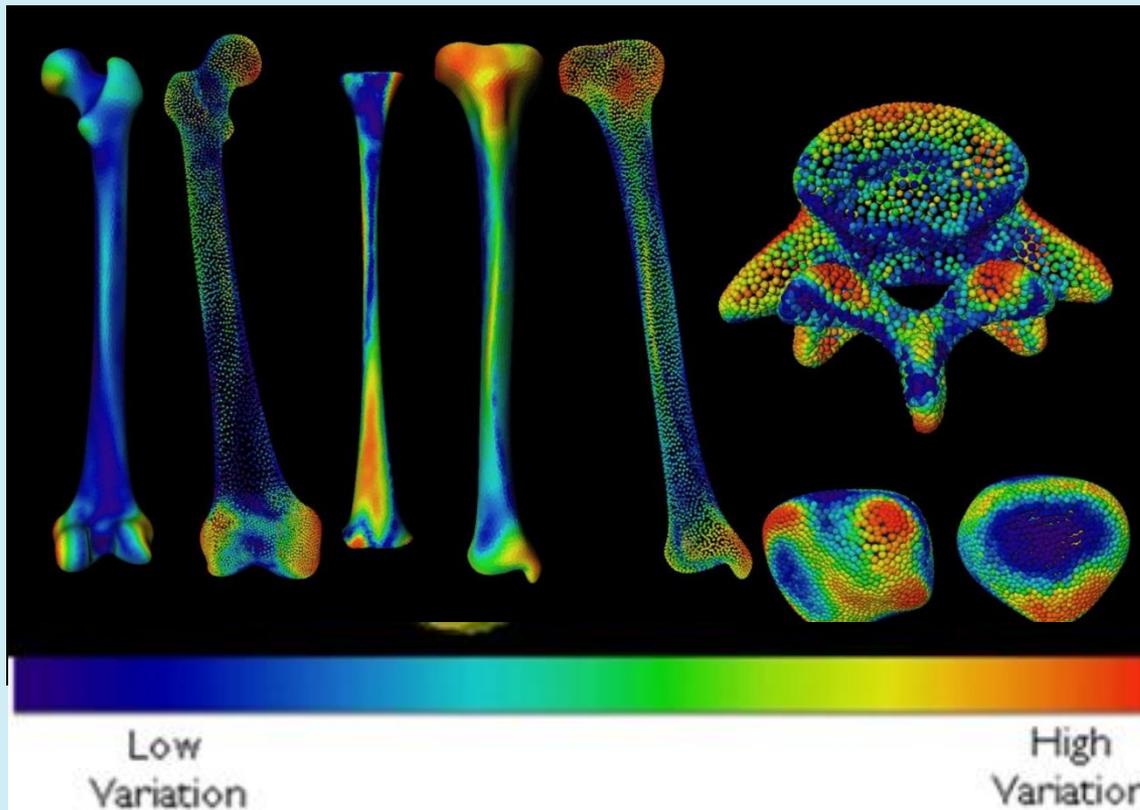
Statistical Representation

- **Landmark-Based**
 - **Disadvantage: manually defined landmarks**
 - **Disadvantage: time-consuming**
 - **Disadvantage: high intraobserver error**
 - ***Only capture local statistics***

- **Surface-Based**
 - **Advantage: performed on entire bone surface after establishing correspondence**
 - **Advantage: quick and convenient method**
 - **Advantage: eliminates subjectivity and only done once**
 - ***Capture both global and local statistics***

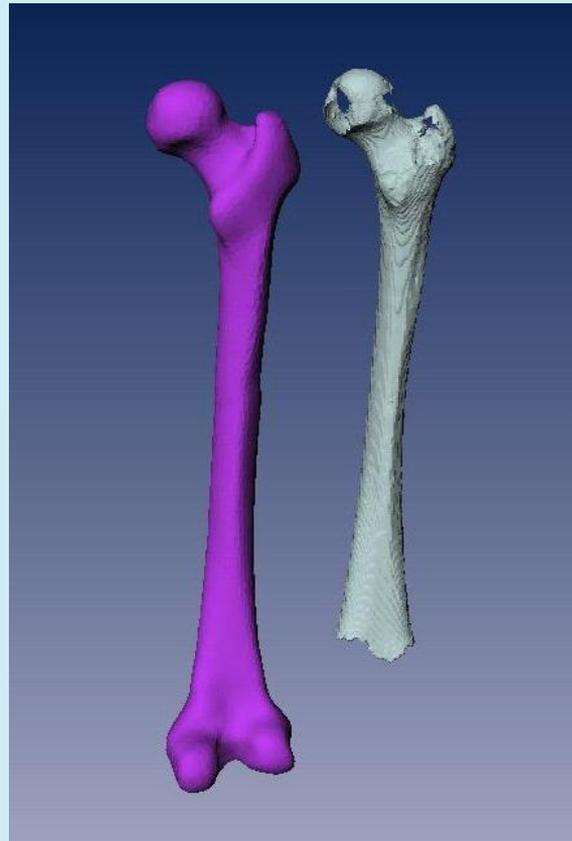
Morphological Differences

- Analysis of differences between gender, ethnicities and ages



Extrapolating Missing Anatomy

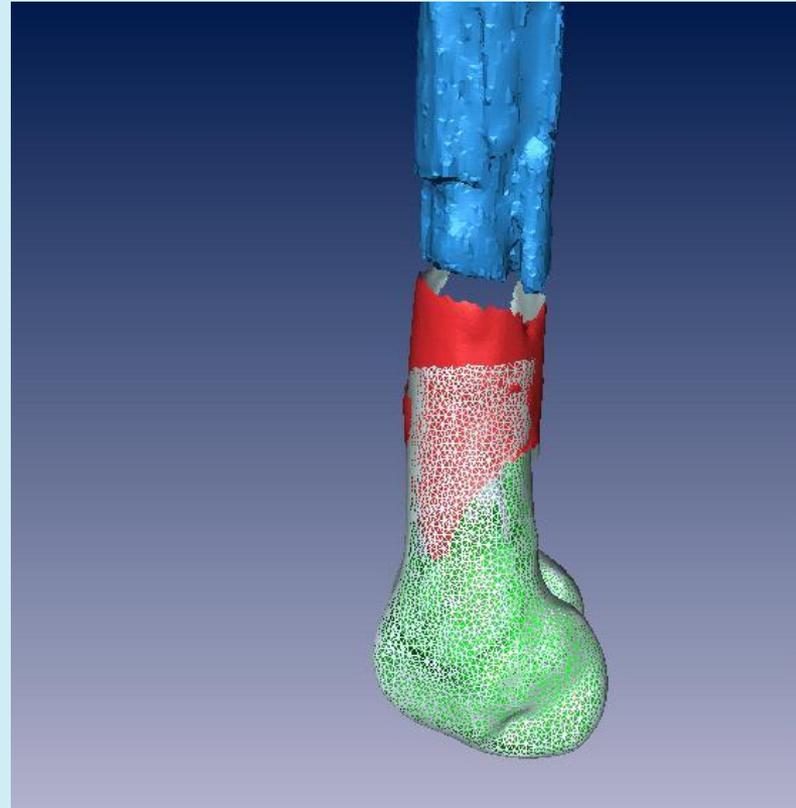
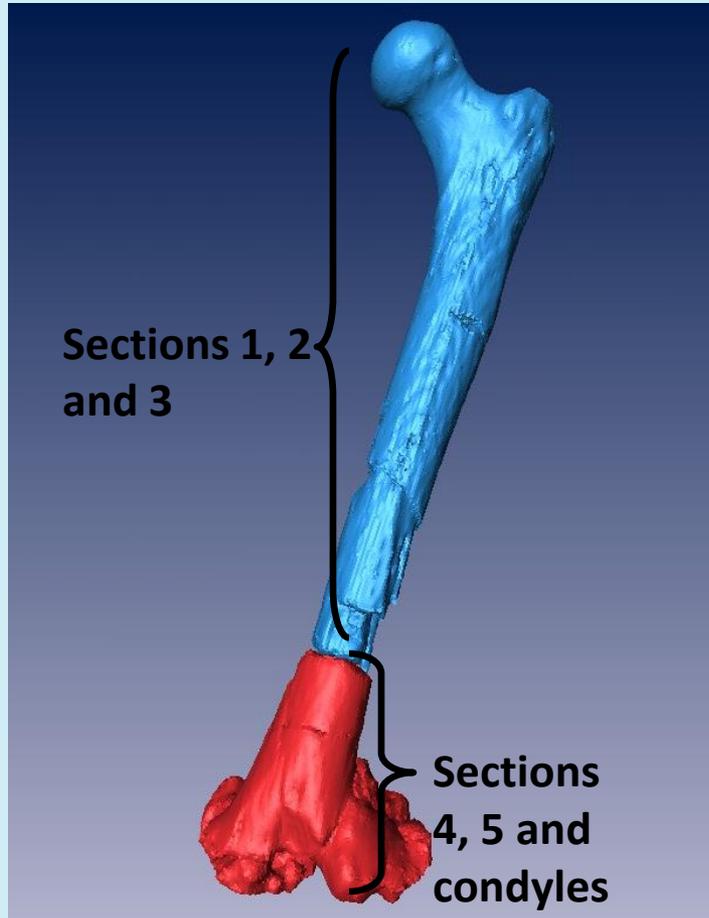
- Extrapolation of missing bone segments



Fragmentary Bone Reconstruction (Traditional By Hand)

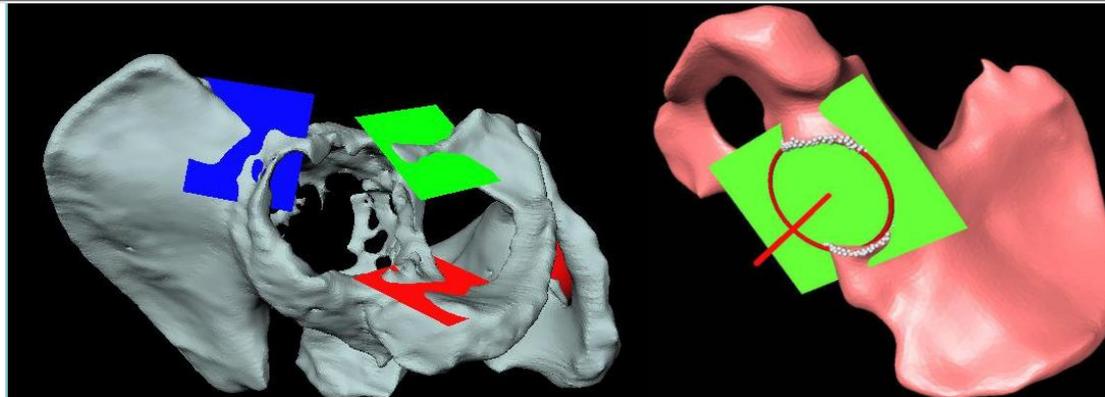
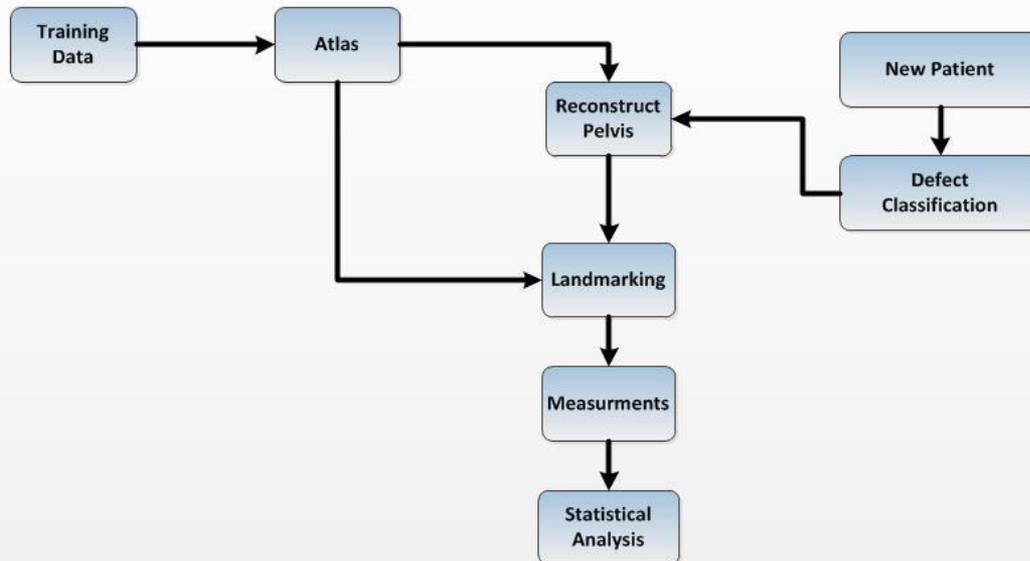


Reconstruction : Conjoinable Pieces

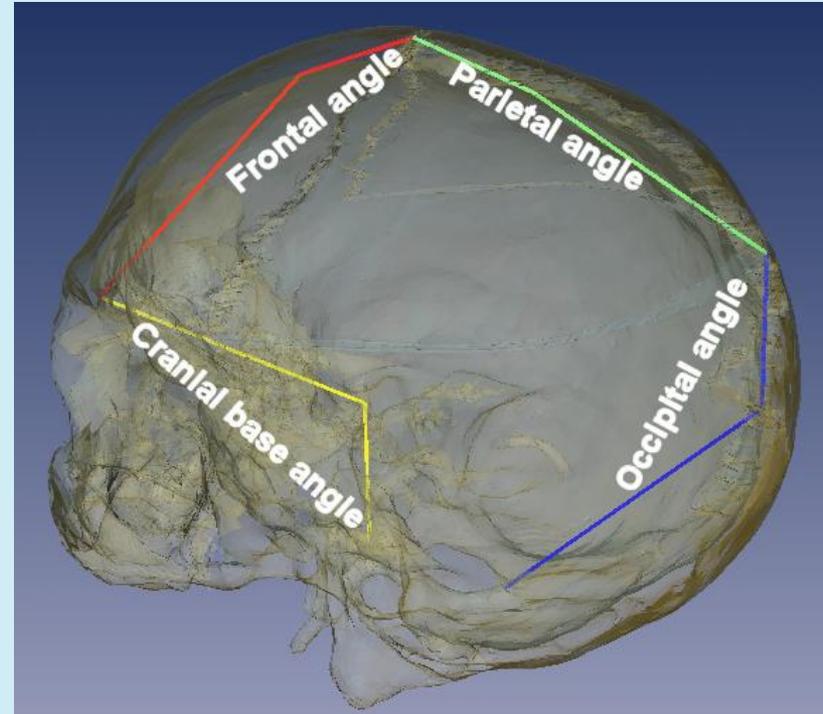
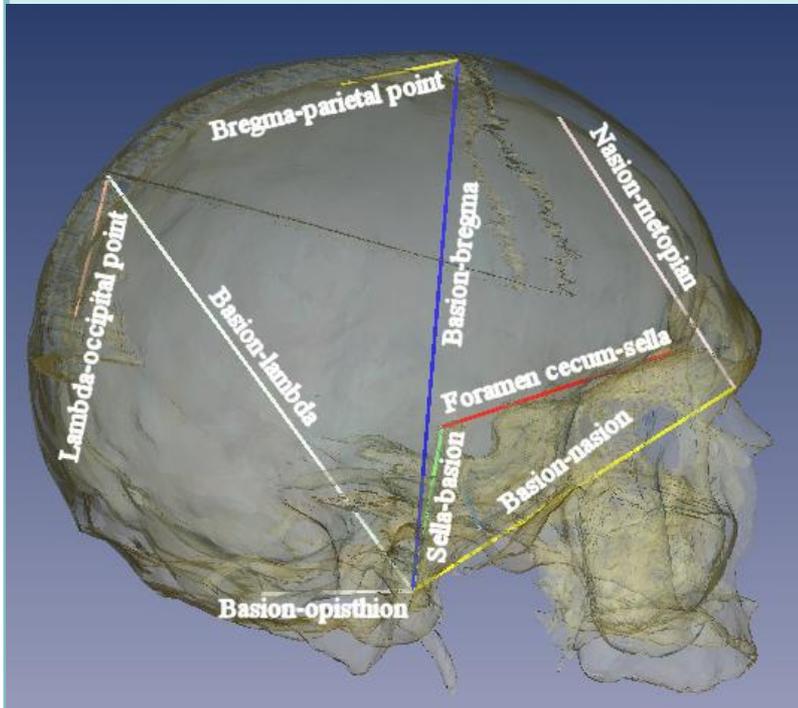


From Sylvester, Merkl and Mahfouz (2008).

Pelvis Reconstruction



Automatic Measurements (Skull)



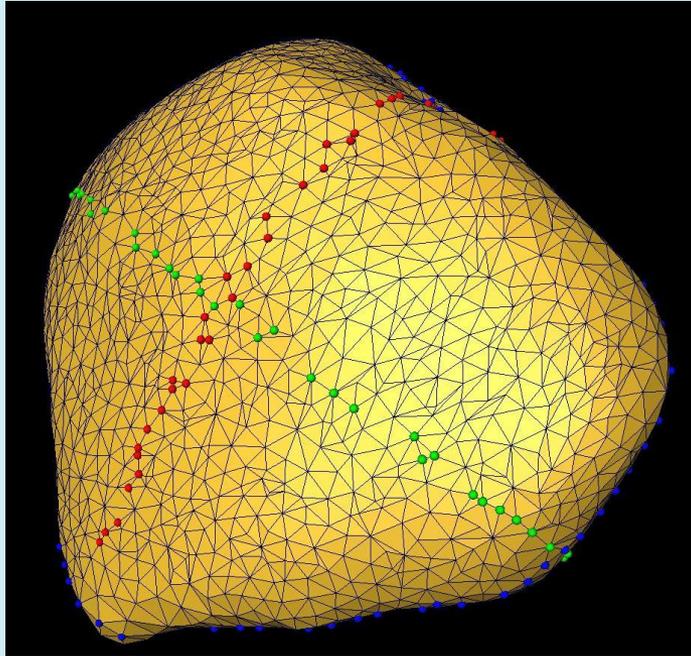
Skull Sexing 98% Using 11 Features

From Shirley, Abdel Fatah, Jantz and Mahfouz (2011).

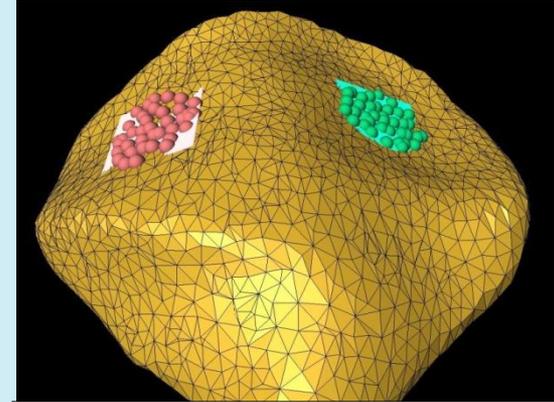
Thickness Measurements (Skull)



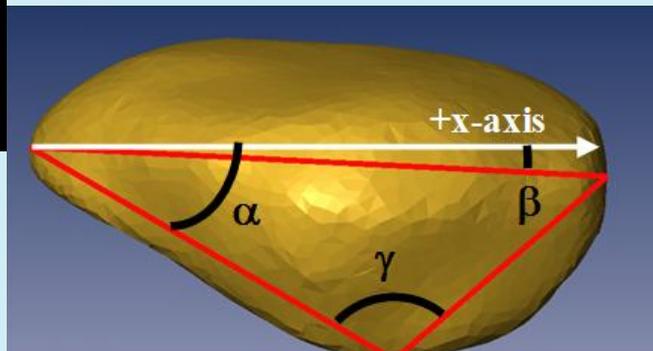
Automated Measurements (Patella)



Circumference Moment Measurements Around 3 Coordinate Axes



Posterior Facet Angle



2D In-plane Measurements

Patella Sexing

Testing results of confusion matrix using a neural network trained on the full 45 features (93.51% correctly classified)

Actual	Predicted		
	Females	Males	Total
Female	28	3	31
Male	2	44	46
Total	30	47	77

From Mahfouz, Badawi, Merkl, Abdel Fatah, Pritchard, Kesler, Moore, Jantz and Jantz (2007).

Cited Scientific References

- Mahfouz, M.R.; Badawi, A.M.; Merkl, B.C.; Abdel Fatah, E.E.; Pritchard, E.; Kesler, K.; Moore, M.K.; Jantz, R.L.; Jantz, L.M. Patella Sex Determination by 3D Statistical Shape Models and Nonlinear Classifiers. *Forensic Science International* 2007, 173(2), 161-170.
- Moore, M.K.; Mahfouz, M.R.; Abdel Fatah, E.E.; Badawi, A.M. Comparison of Dry and In Vivo Bone Densities from CT Images using Fuzzy Logic and Neural Networks. *Computer Methods in Biomechanics and Biomedical Engineering, 7th International Symposium, Cote De Azure, France, 2006.*
- Shirley, N.R.; Abdel Fatah, E.E.; Jantz, R.L.; Mahfouz, M.R. Improving Sex Estimation from the Human Cranium Using 3D CT Scans. *American Academy of Forensic Sciences, 63rd Annual Scientific Meeting, Chicago, IL, 2011.*
- Sylvester, A.D.; Merkl, B.C.; Mahfouz, M.R. Reconstructing the AL 288-1 Femur Using Three-Dimensional Computer Models. *Journal of Human Evolution* 2008, 55, 665-671.

Questions?

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